

Likelihood Analysis of Diffusion Weighted MRI

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BIRN

BIOMEDICAL INFORMATICS RESEARCH NETWORK

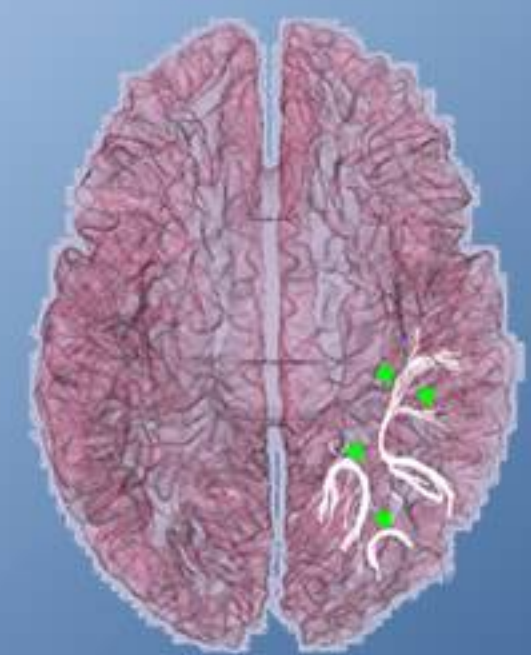
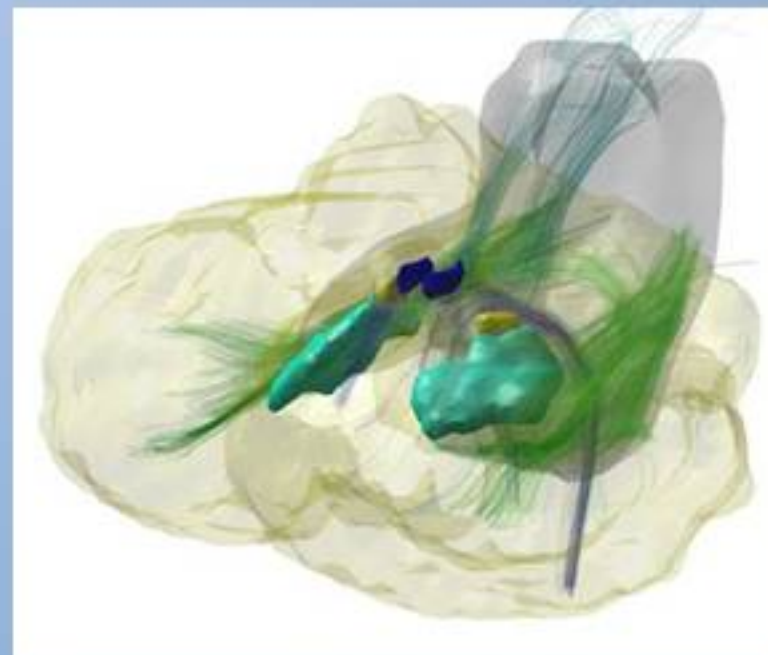
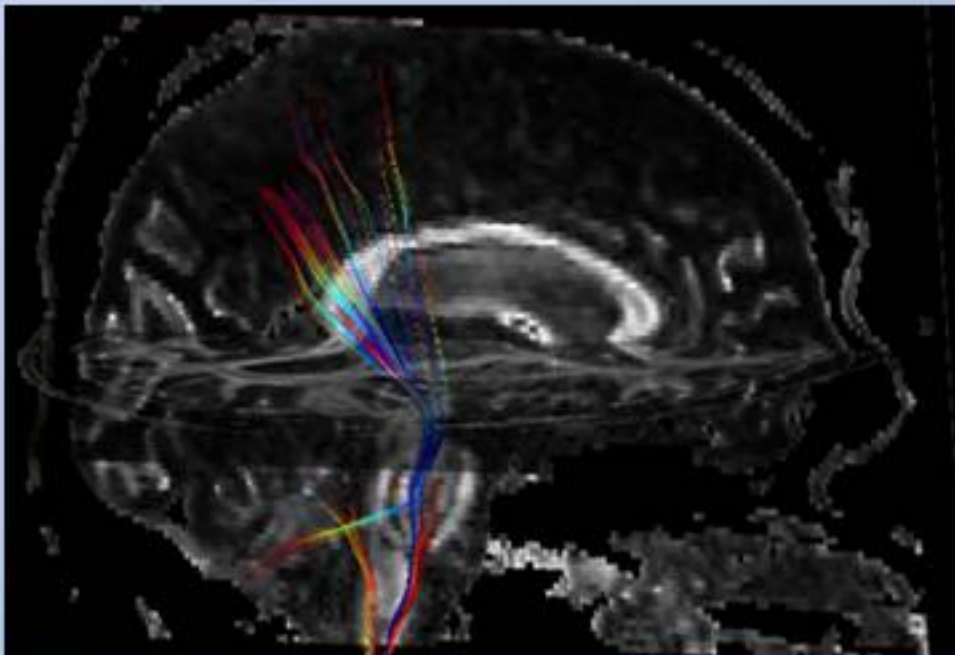
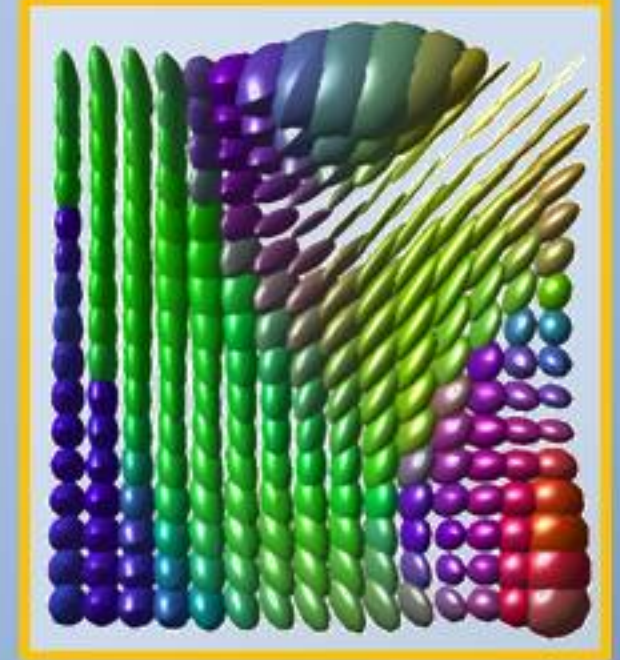
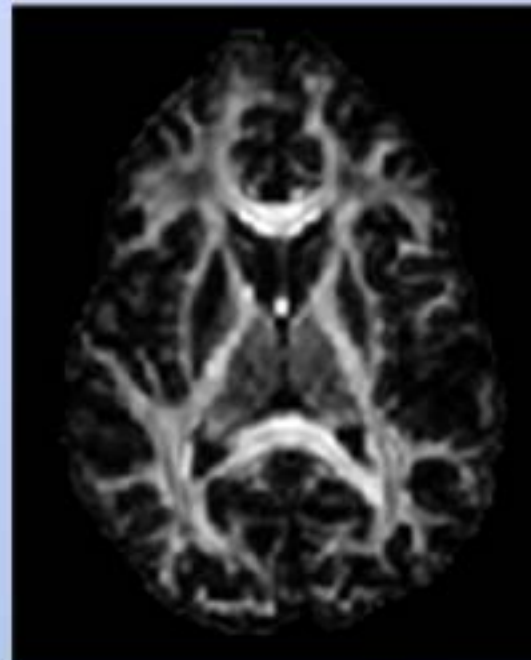
MEDIC



Kennedy Krieger Institute

*E.M. Kirby Research Center for
Functional Brain Imaging*

Revealing Tissue Architecture

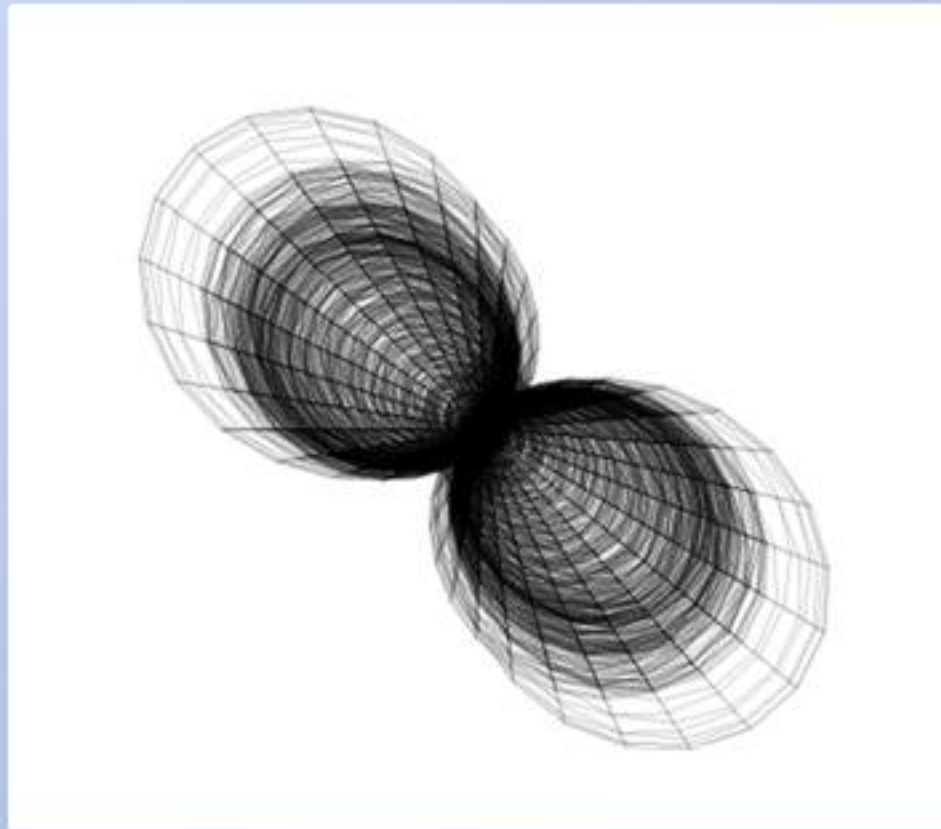


Noise Corrupts Estimated Structure

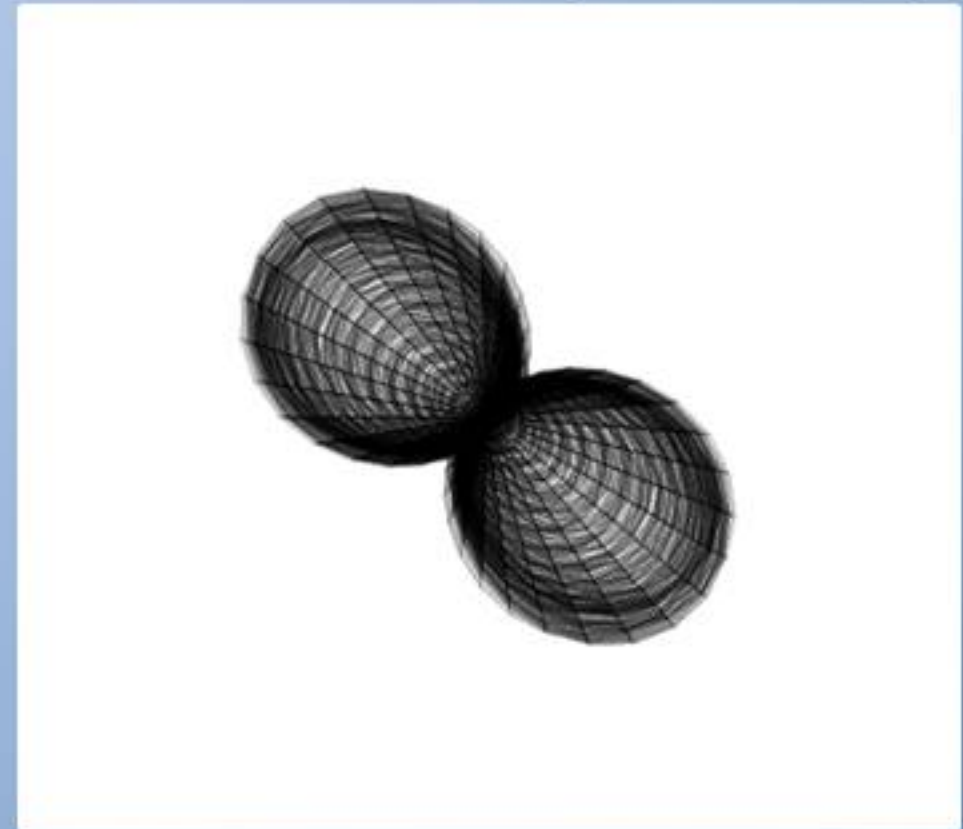
Landman et al. 2008a

One White Matter Voxel Scanned 22 Times Over 3 Days

Traditional Estimator

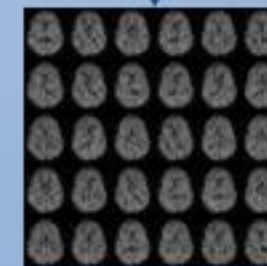


Robust Estimator (Likelihood)

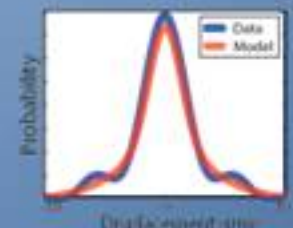
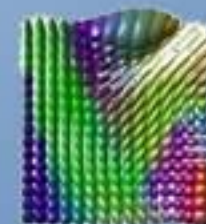


Overview

- **Background**
- Signal and Noise in DW-MRI
- Diffusion Tensor Imaging
- Q-Space Imaging
- Conclusion
- Future Directions

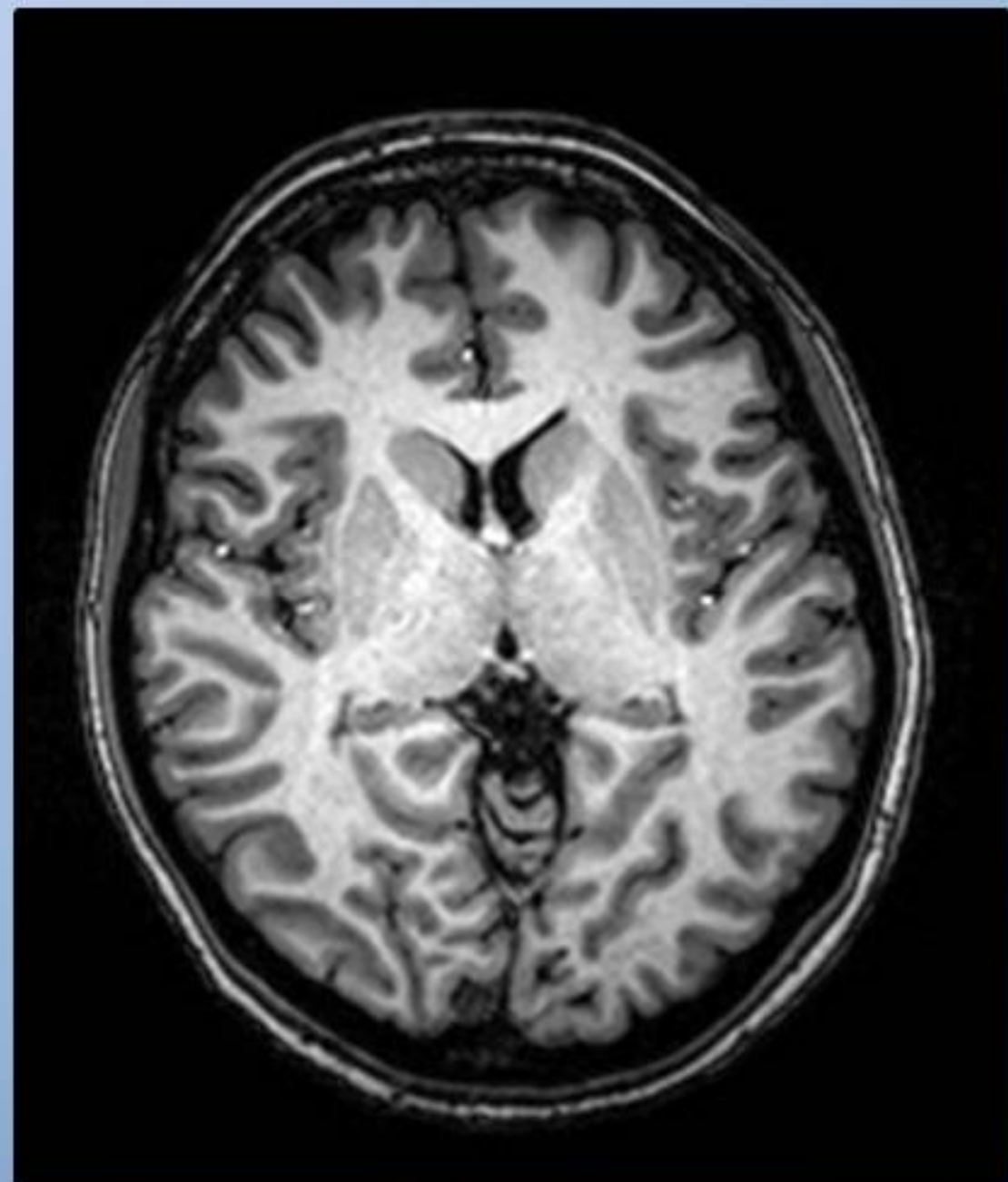
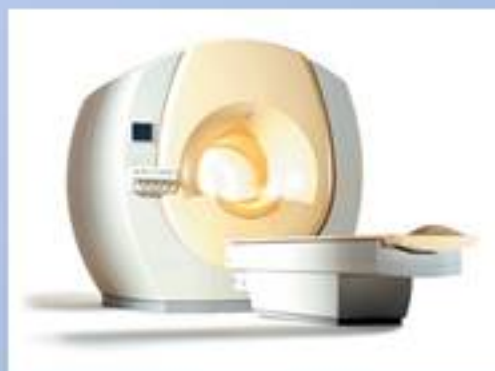


σ



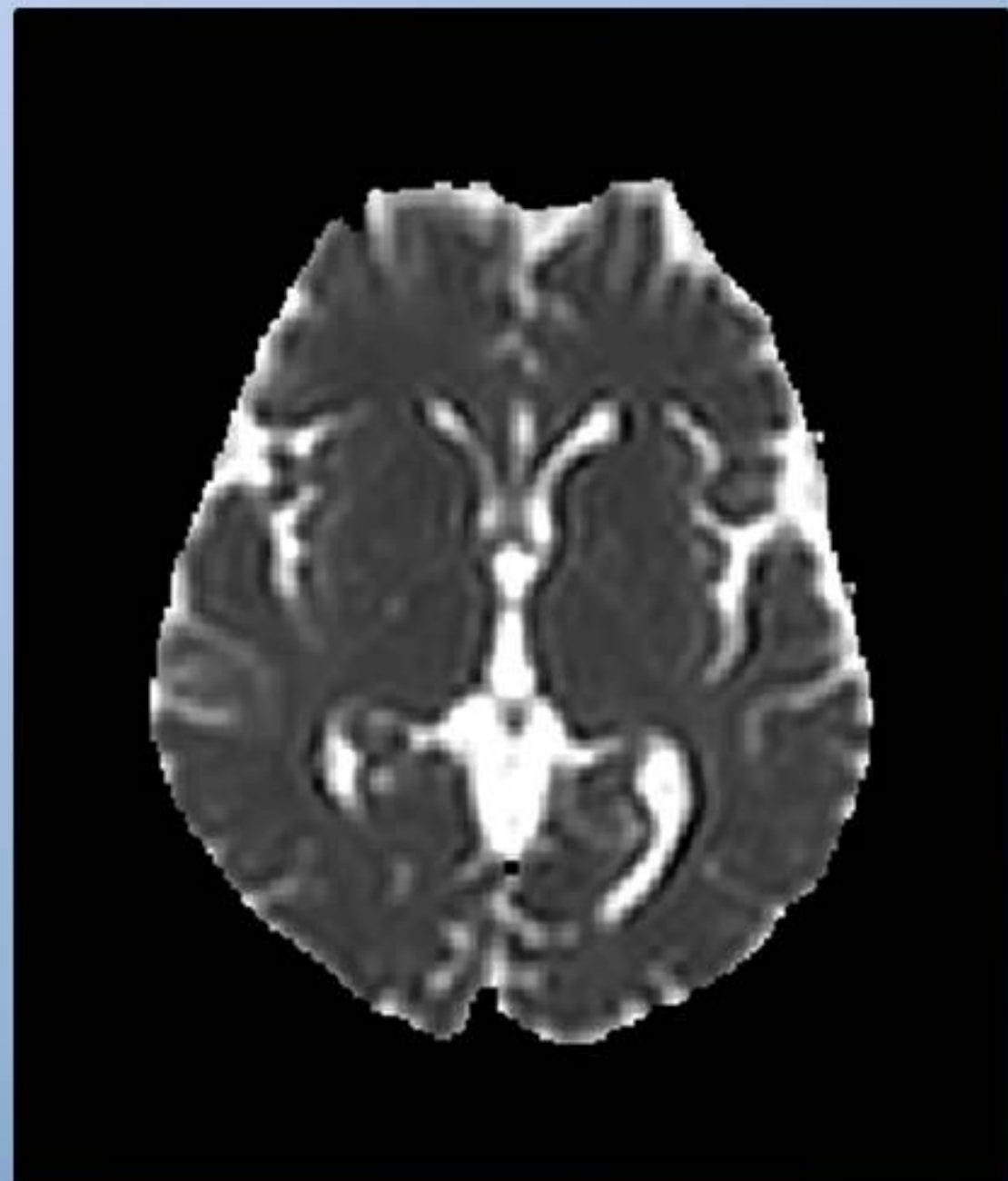
Structural MRI

- **Contrast dominated by**
 - NMR properties
 - T1, T2, PD
- **White matter appears relatively homogeneous**



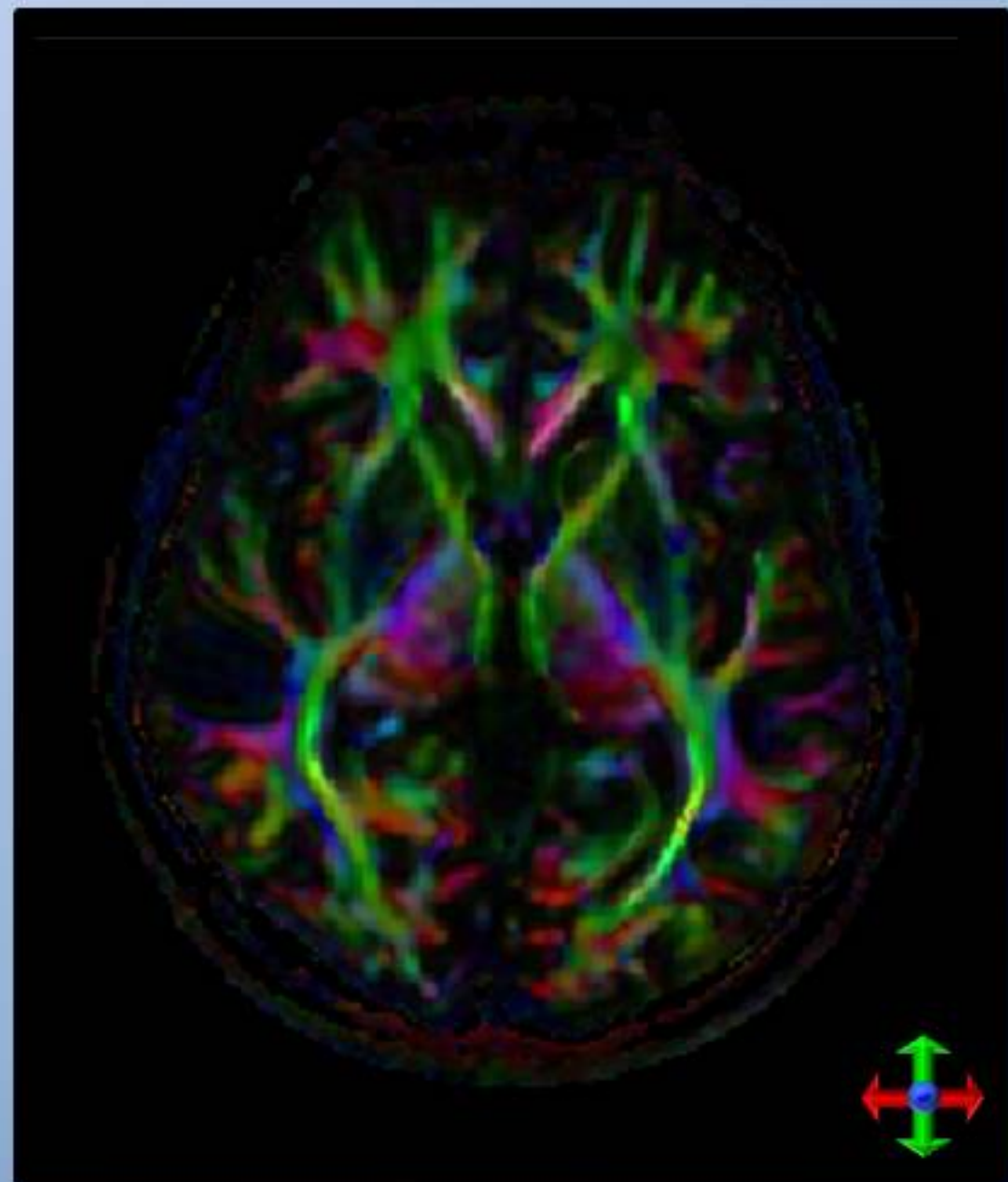
Diffusion Weighted MRI

- **Does water diffuse?**
 - Depends on tissue
 - Greatest diffusion in cerebrospinal fluid
- **Mean diffusivity is nearly constant**



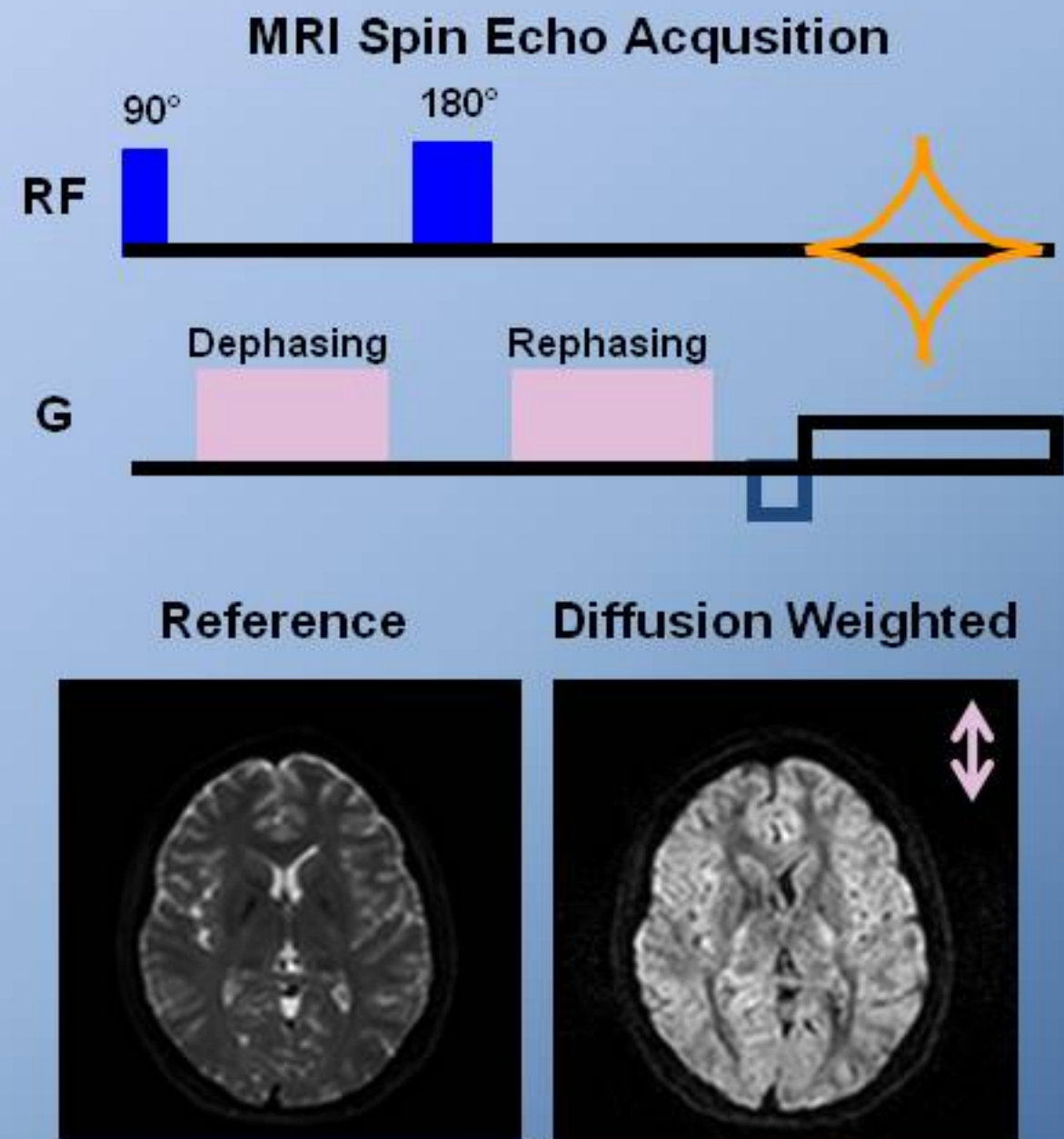
Directional Diffusion

- **Preferred direction?**
 - Diffusivity
 - Orientation
 - Anisotropy...
- **Derived Quantities**



Measuring Diffusion

- **Sensitize to diffusion with balanced gradient pulses**
 - No Motion → No Effect
 - Bulk (Coherent) Motion → Phase Shift
 - **Diffusion (Incoherent) Motion → Signal Loss**



Accounting for Signal Loss

Cory & Garroway 1990

$$\begin{aligned}
 S(\underbrace{\mathbf{q}}_{\text{Weighting Factor}}, \underbrace{\Delta}_{\text{Diffusion Time}}) &= S_0 \left| \int_{\mathbf{r}_0} \int_{\mathbf{r}} \rho(\mathbf{r}) \underbrace{\mathbf{P}(\mathbf{r}|\mathbf{r}_0, \Delta)}_{\text{Motion Probability "Propagator"}} \right. \\
 &\quad \times \underbrace{\exp [j2\pi \mathbf{q} \cdot (\mathbf{r} - \mathbf{r}_0)]}_{\text{Phase change due to motion from } \mathbf{r} \text{ to } \mathbf{r}_0} \left. \right|
 \end{aligned}$$

Sum over Volume and Number of Spins
 Ref. Motion

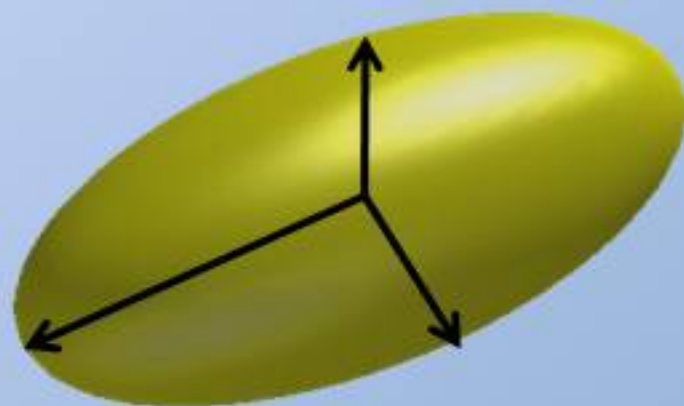
Note (units: 1/length):

$$\mathbf{q} = \frac{1}{2\pi} \gamma \mathbf{g} \delta$$

Motion Probability Propagators

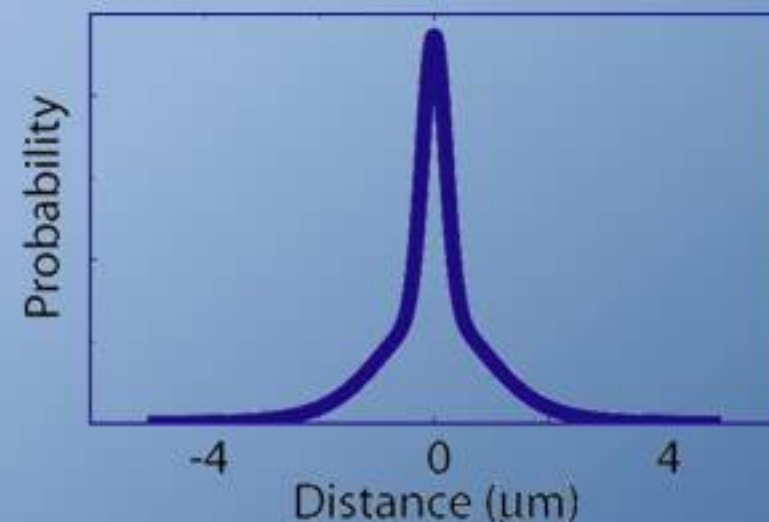
Diffusion Tensor MRI

- 3-D Gaussian
 - *Diffusion by direction*
 - Integrity and connectivity
 - Tensor ellipsoids



Q-Space MRI

- 1-D Nonparametric
 - *Diffusion by displacement*
 - Restriction environment
 - Probability density functions



Where Does the Signal Come from?

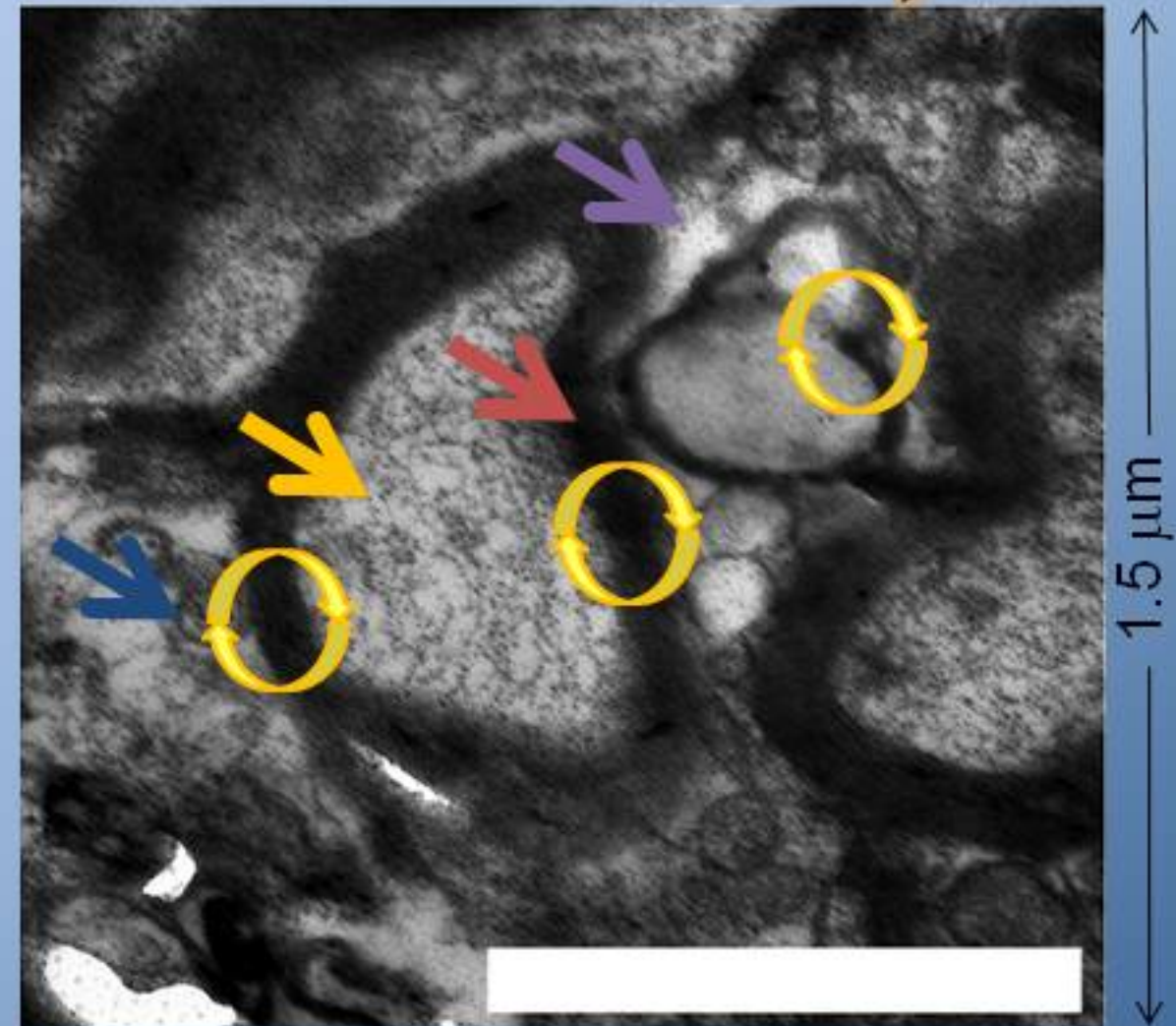
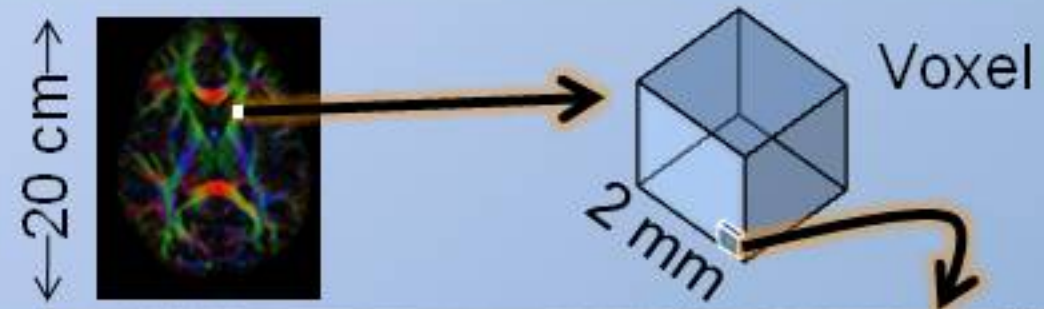
- **Sources of signal**

- Intra-axonal →
- Myelin →
- Extra-cellular →
- Intra-glia →

- **All of the above!**

- Apprx. 5.2×10^{20} water protons/voxel

- And **exchange!** ○



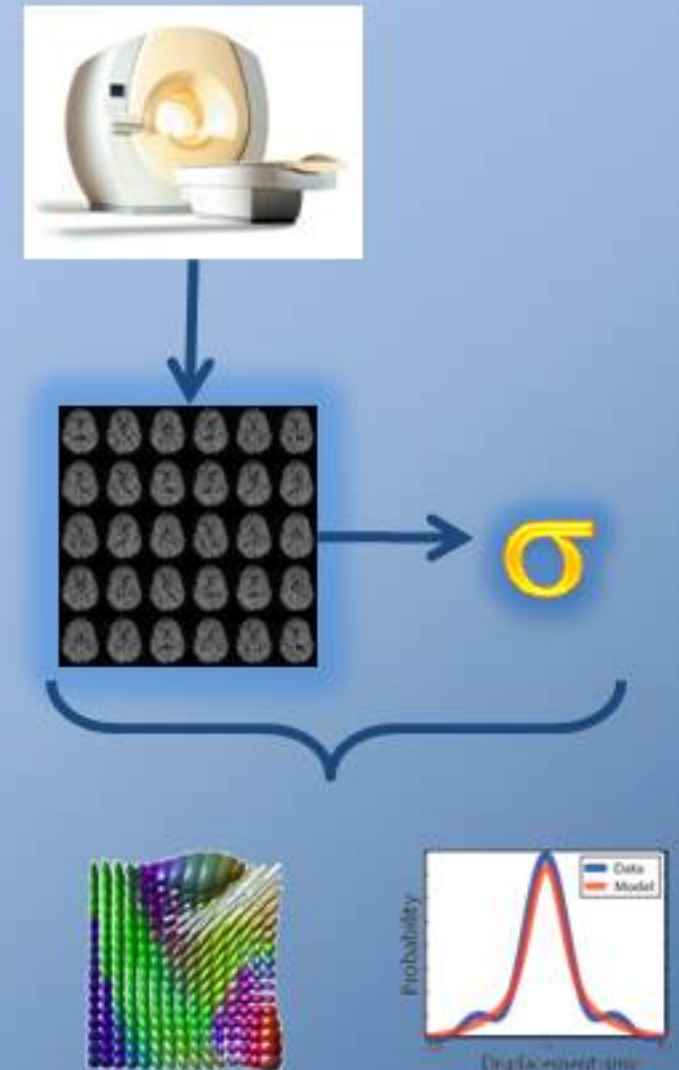
Likelihood in DW-MRI

$\mathcal{L}(\text{observations}; \text{acquisition, propagator})$

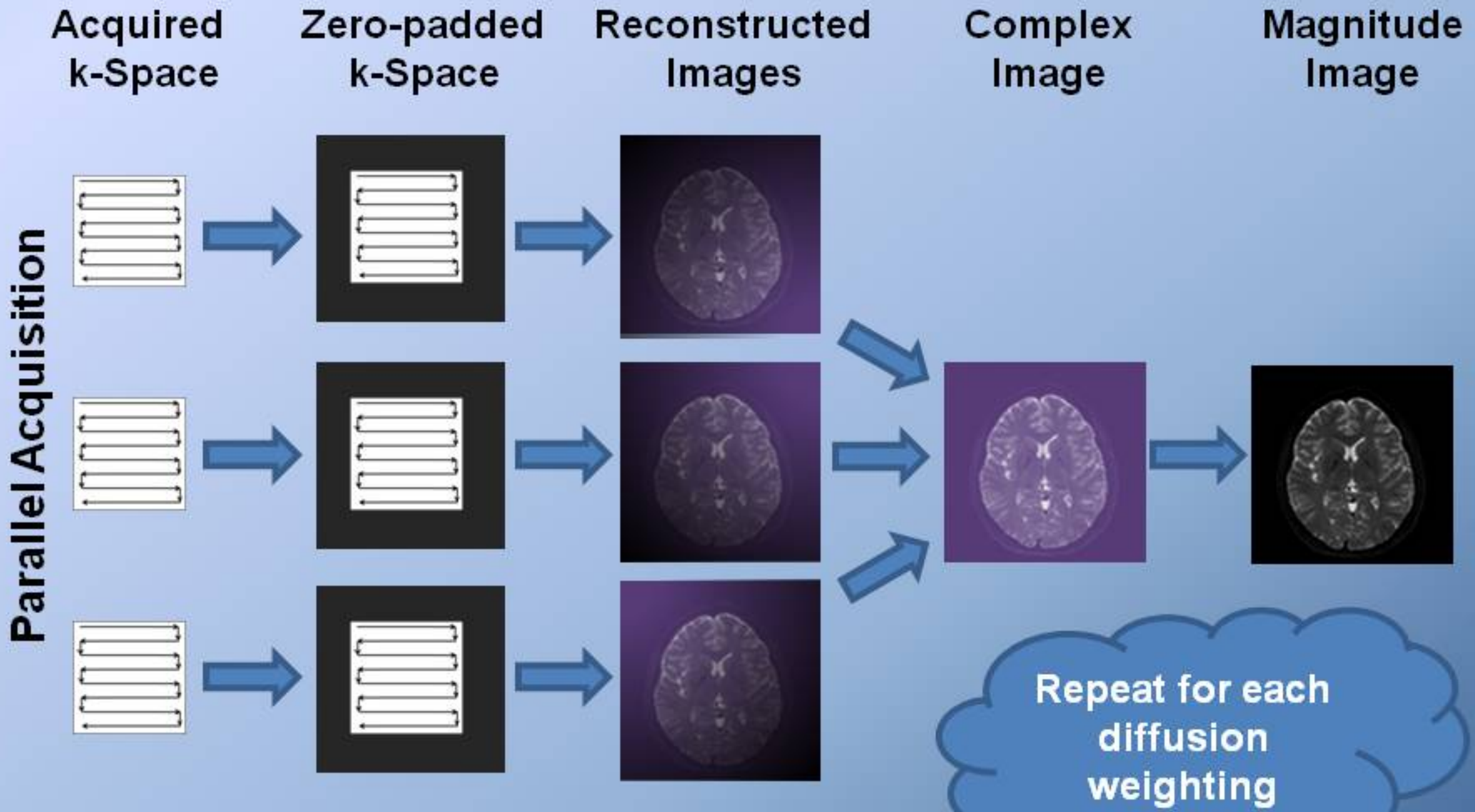
- Explain and account for diffusion behavior of water protons *in vivo*
 - Understand the acquisition (signal theory)
 - Model diffusion propagator

Overview

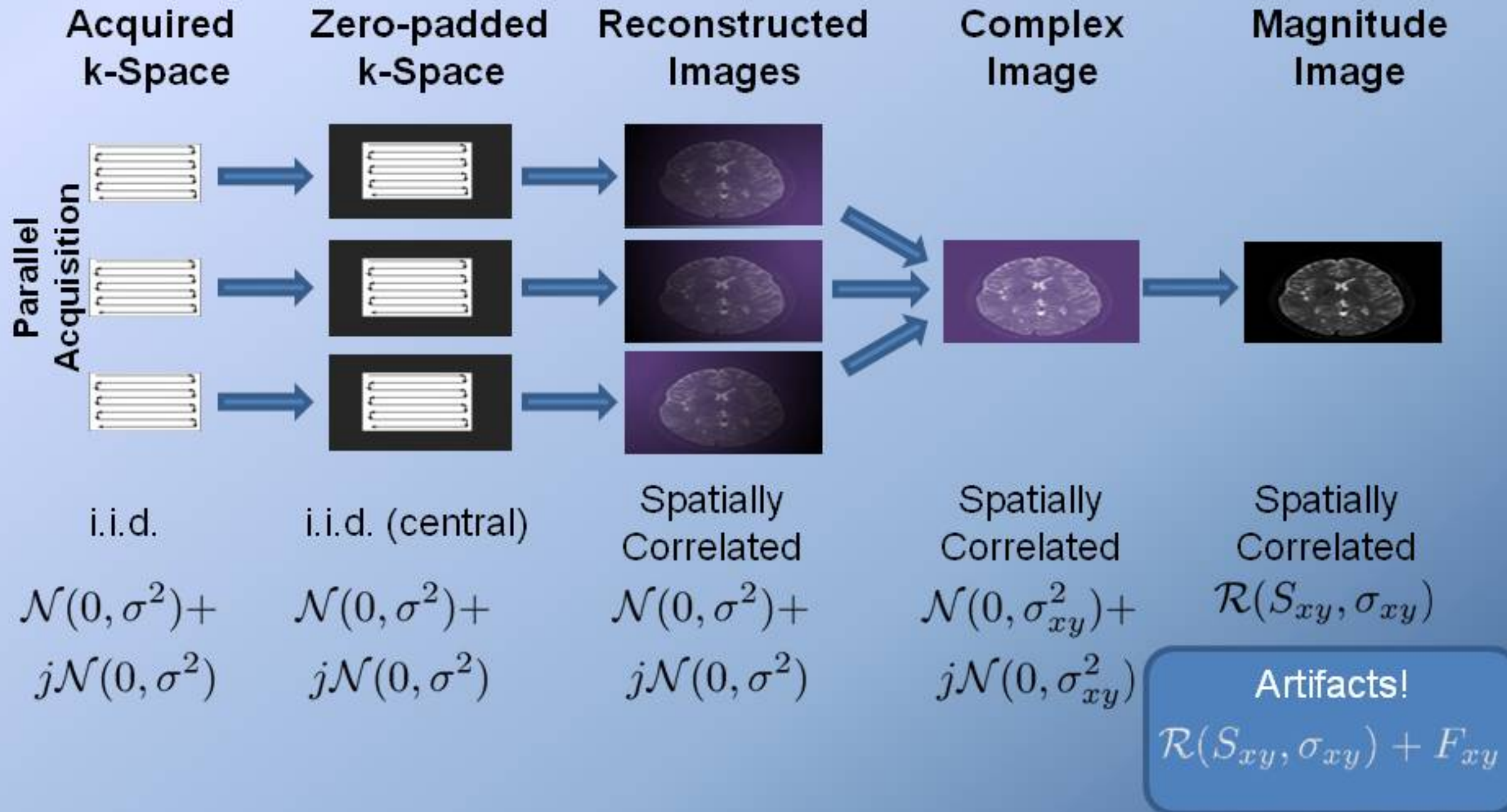
- Background
- **Signal and Noise in DW-MRI**
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Inside the Scanner

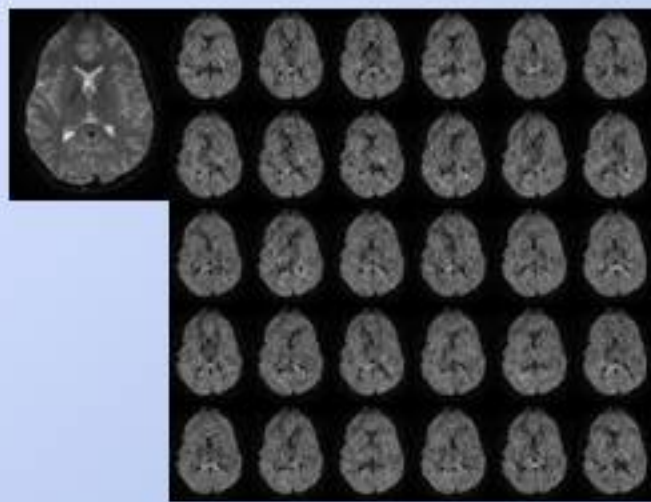


Noise Propagation

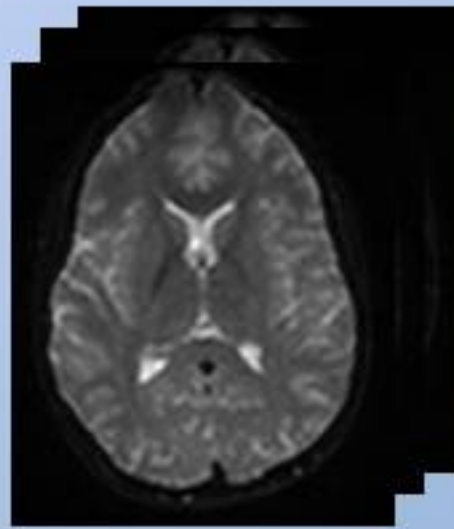


Outside the Scanner

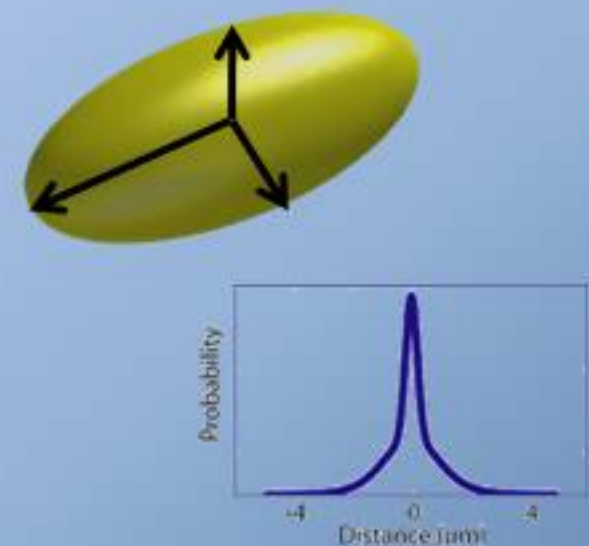
Acquired Data



Motion Corrected



Diffusion Model



Diffusion Images i.i.d.
Spatially Correlated

$$\mathcal{R}(S_{gxy}, \sigma_{xy}) + F_{xy}$$

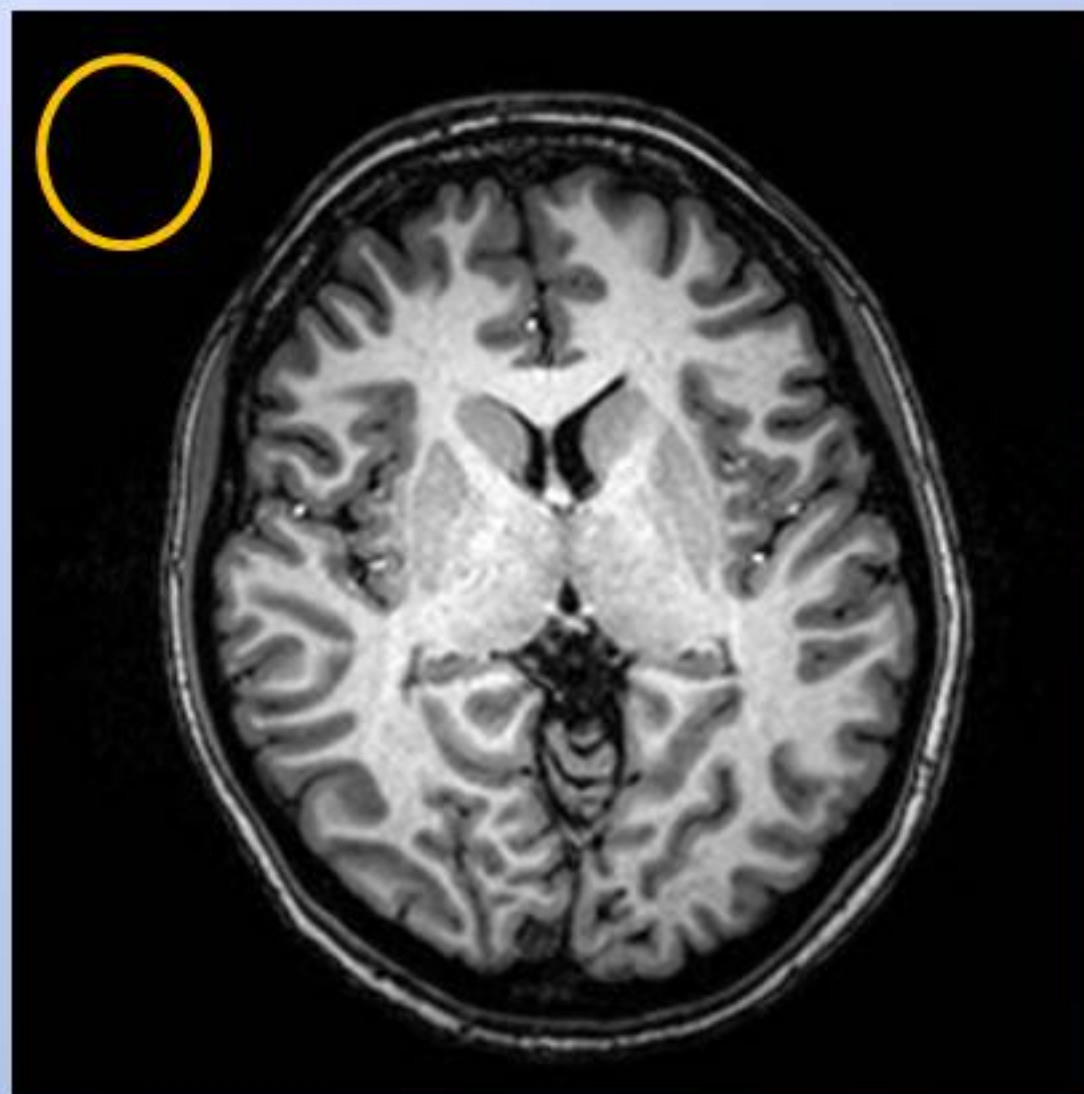
Diffusion Images i.i.d.
Spatially Correlated

$$\mathcal{R}(S_{gxy}, \sigma_{xy}) + \tilde{F}_{xy}$$



Traditional Noise Estimation

Kaufman et al. 1989



Traditional Method

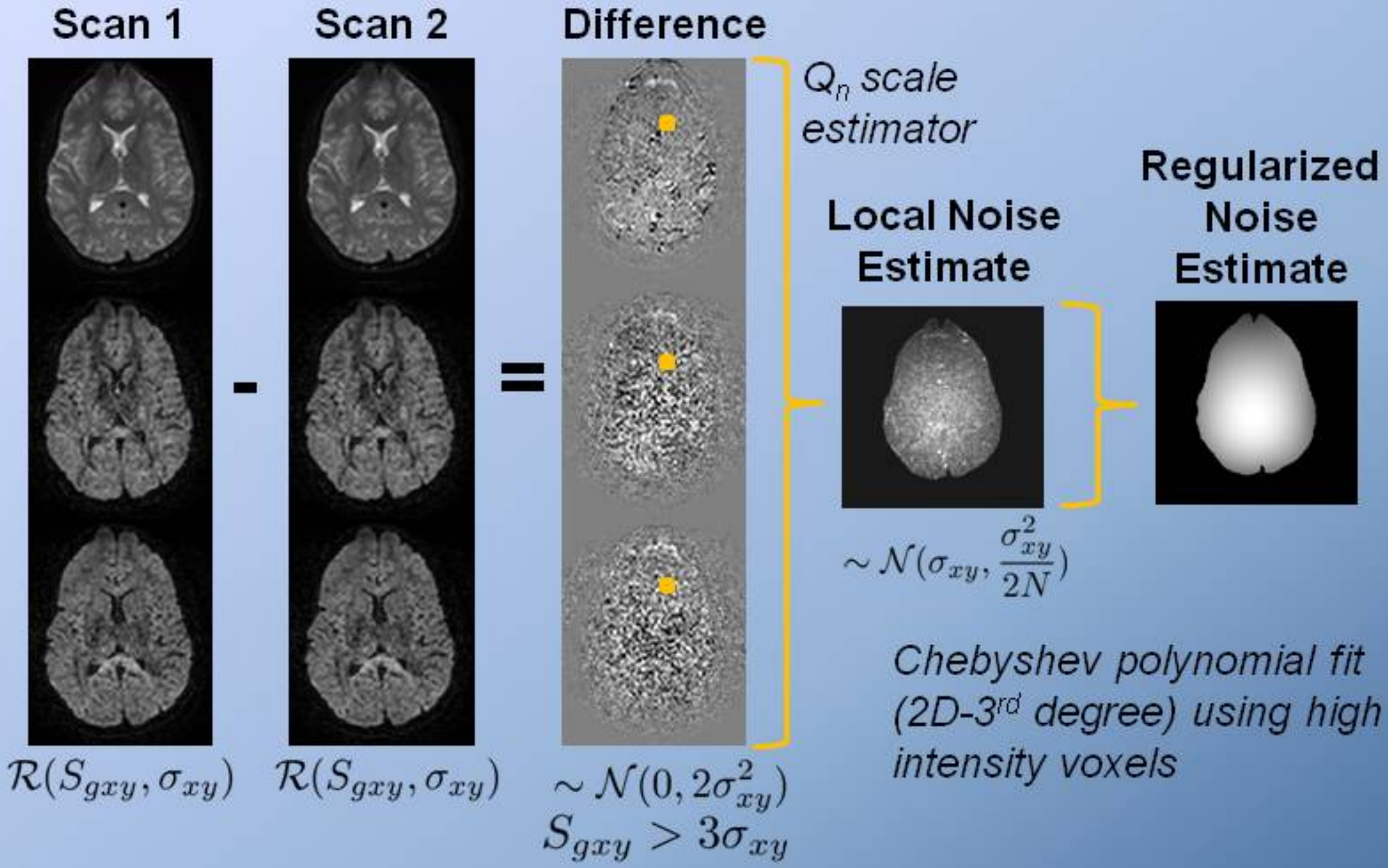
- Select a background region
- Rician \rightarrow Rayleigh in absence of signal

Challenges

- **Spatially varying noise**
 - Parallel imaging
- Correlated noise
 - Up-sampling
- Non-representative background
 - Ghosting artifacts
 - Background suppression
- Limited time available for clinical sequences

Robust Noise Estimation

Landman et al. 2007a,2008b



How Can We Validate?

- **Map Noise Field vs. Traditional Scalar Methods**
 - Compare median field estimate
- **Simulation**
 - What is the predicted accuracy?
- **Phantom**
 - How does noise level correlate with the number of signal averages?
- ***In vivo***
 - How do estimates based on clinical data compare to ground truth noise levels?

Validation

- **Simulation**

- 100x more accurate when accounting for spatially variable noise and artifacts

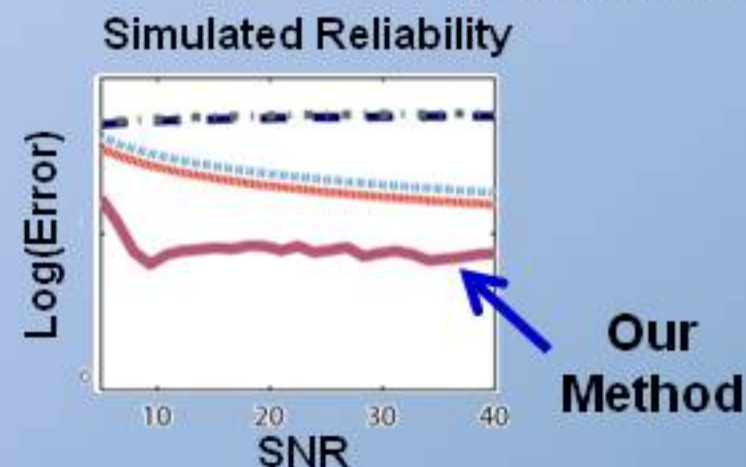
- **Phantom**

- In agreement with theory: $R^2=0.99$
- Other methods: $R^2 \leq 0.95$

- ***In vivo***

- Spatially consistent with ground truth estimates ($\sim 5\%$)
- Mean estimate within $1.7 \pm 0.9\%$
- Other methods: $\geq 11.2 \pm 1.9\%$

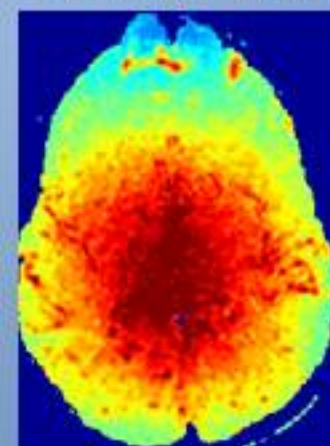
Landman et al. 2008b



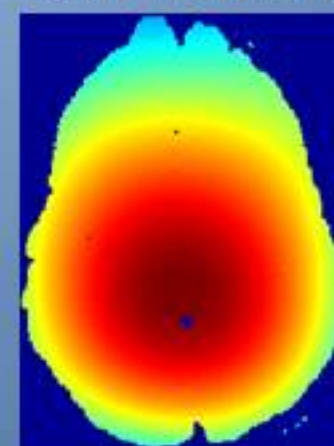
Averages



Ground Truth

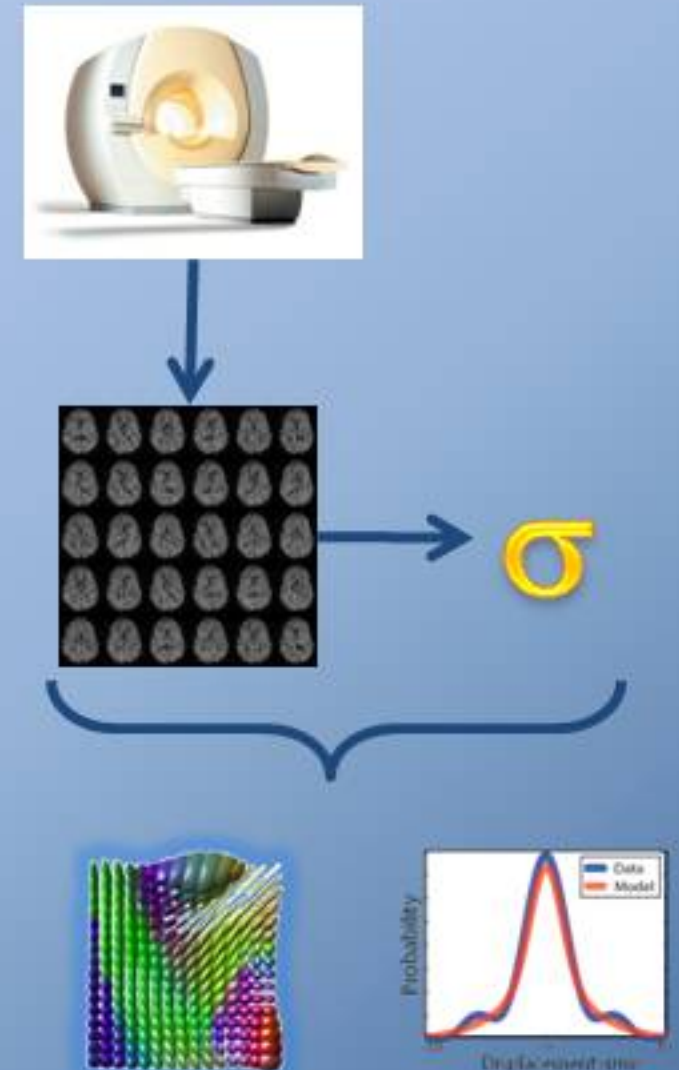


Our Method



Overview

- Background
- Signal and Noise in DW-MRI
- **Diffusion Tensor Imaging**
- Q-Space Imaging
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- Future Directions



Stejskal-Tanner Tensor Model

Stejskal & Tanner 1965

Signal Attenuation

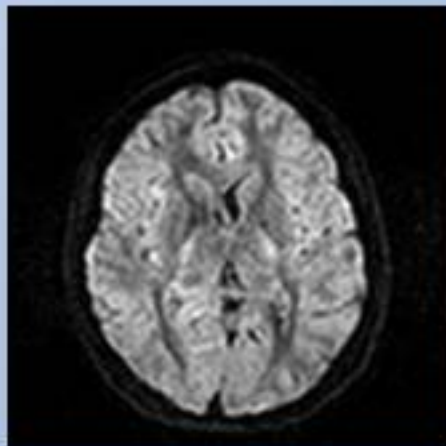
$$S(\mathbf{q}, \Delta) = S_0 \left| \iint \rho(\mathbf{r}_0) \mathbf{P}(\mathbf{r}_0 | \mathbf{r}, \Delta) \right. \\ \left. \times \exp[j2\pi \mathbf{q} \cdot (\mathbf{r} - \mathbf{r}_0)] \right|$$



b-value Gradient
 $b = |\mathbf{q}|^2 \Delta$ orientation

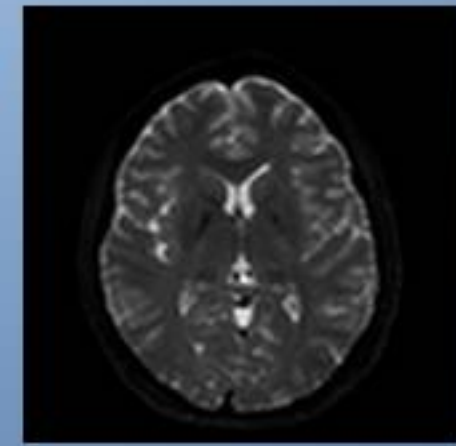
Diffusion
 tensor

$$S(b, \mathbf{g}) = S_{\text{ref}} e^{-b \mathbf{g}^T \mathbf{D} \mathbf{g}}$$



Signal with
 diffusion
 weighting

Signal without
 diffusion
 weighting



Visualizing Tensors

$$D = \begin{bmatrix} D_{xx} & D_{xy} & D_{xz} \\ D_{xy} & D_{yy} & D_{yz} \\ D_{xz} & D_{yz} & D_{zz} \end{bmatrix}$$



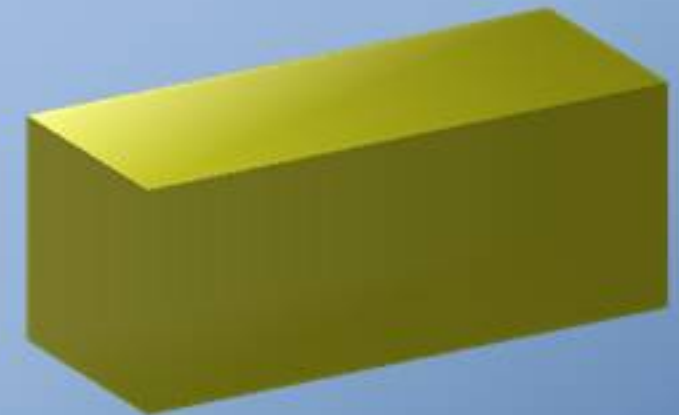
Diffusion Peanut

Distance from the origin represents apparent diffusivity in each orientation



Diffusion Ellipsoid

Surface is an isosurface of the probability of diffusion



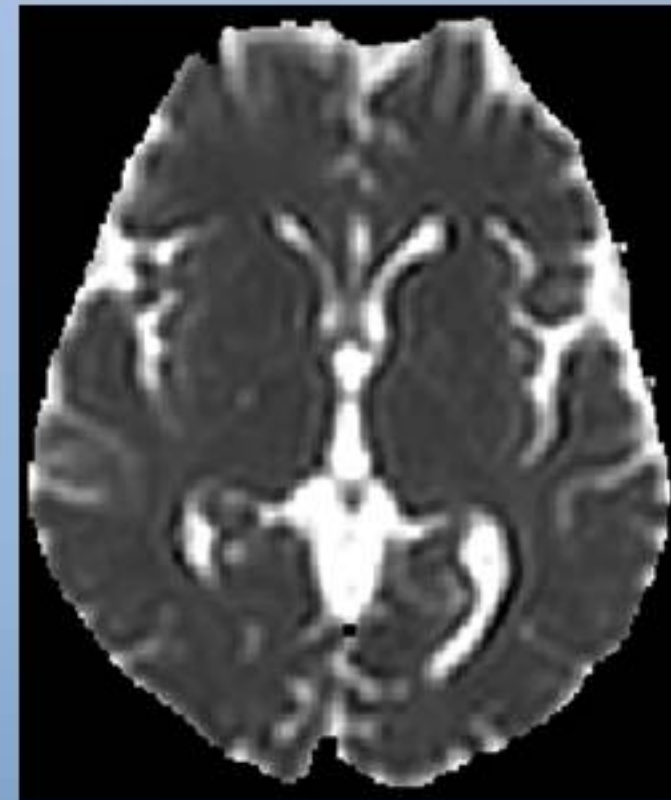
Diffusion Box

Length of edges represents the diffusivity along the principle axes

Diffusivity

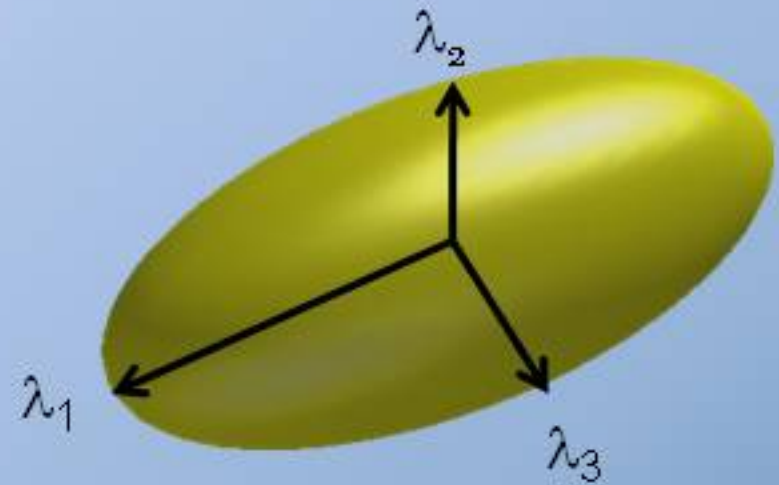
- “Apparent diffusion coefficient” varies by direction: ADC_g
- Need an “invariant” metric
- Solution:
 - Mean diffusivity
 - Apparent diffusion coefficient
 - Tensor trace

$$\begin{aligned}ADC = MD &= \frac{\text{tr}\mathbf{D}}{3} \\ &= \frac{\lambda_1 + \lambda_2 + \lambda_3}{3}\end{aligned}$$



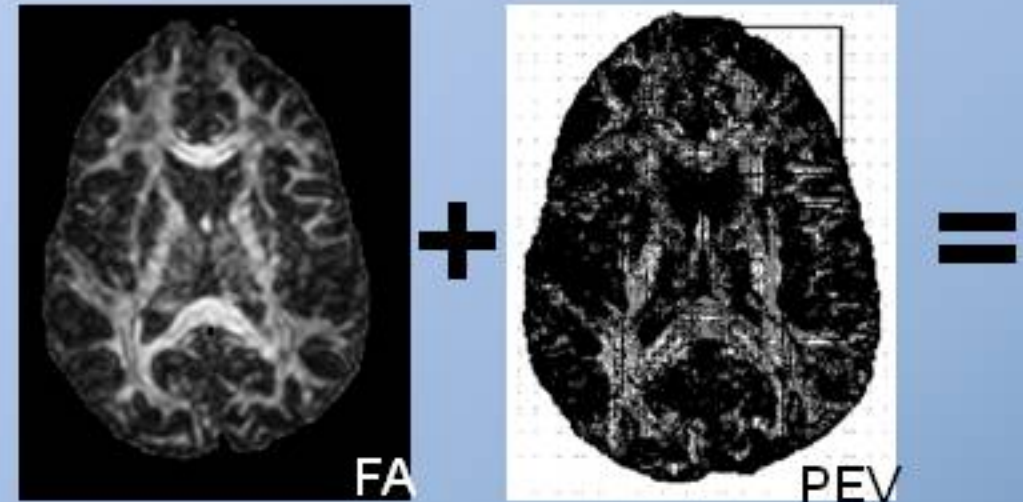
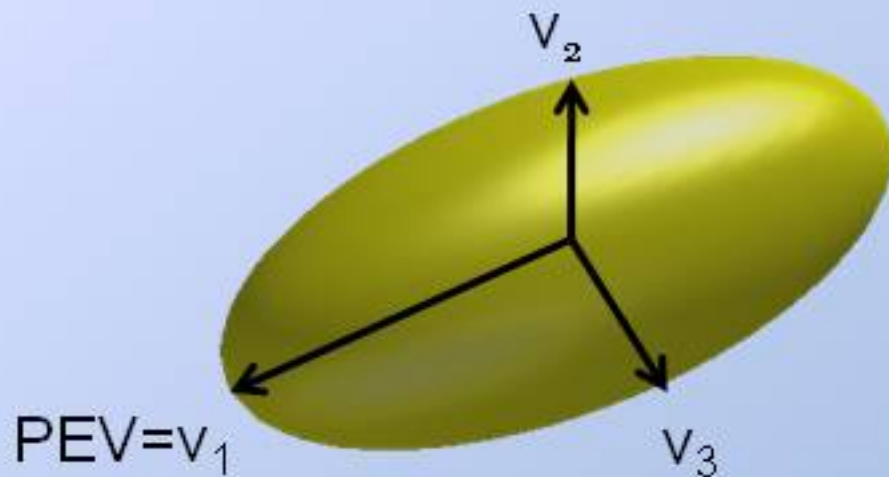
Anisotropy

- First Metrics
 - “Ratios” of Eigenvalues
 - Sorting Problem
- Invariant Metrics
 - Relative Anisotropy
 - Lattice Index
 - **Fractional Anisotropy (FA)**



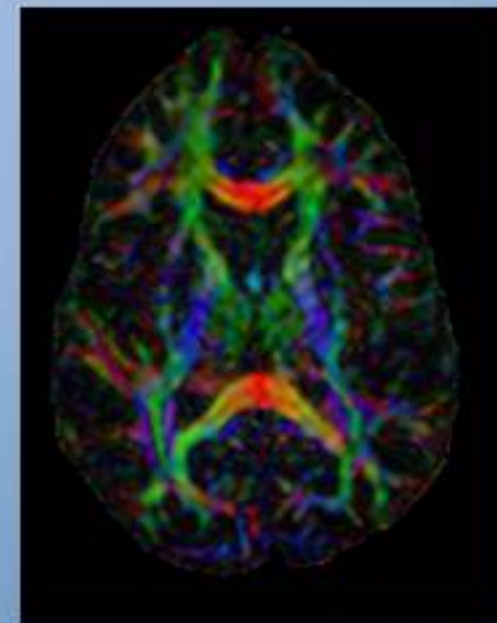
$$FA = \sqrt{\frac{3}{2} \frac{(\lambda_1 - \bar{\lambda})^2 + (\lambda_2 - \bar{\lambda})^2 + (\lambda_3 - \bar{\lambda})^2}{\lambda_1^2 + \lambda_2^2 + \lambda_3^2}}$$

Orientation



Color-coded Diffusion Maps

- Pure red: left to right
- Pure green: front to back
- Pure blue: head to foot
- Colors blended by direction
- Intensity multiplied by FA



Estimating Tensors

Basser & Jones 2002

- Relation of ADC to tensor elements

$$\begin{aligned}
 \text{ADC}_{\mathbf{g}} &= -\frac{1}{b} \ln \frac{S_{\text{dw}}}{S_{\text{ref}}} \\
 &= \mathbf{g}^T \mathbf{D} \mathbf{g} \\
 &= [g_x^2 \ 2g_x g_y \ 2g_x g_z \ g_y^2 \ 2g_y g_z \ g_z^2] [D_{xx} \ D_{xy} \ D_{xz} \ D_{yy} \ D_{yz} \ D_{zz}]^T \\
 &= \mathbf{G}_{\mathbf{g}} [D_{xx} \ D_{xy} \ D_{xz} \ D_{yy} \ D_{yz} \ D_{zz}]^T
 \end{aligned}$$

- Least squares (LS) estimate (Gaussian Noise):

$$[\hat{D}_{xx} \ \hat{D}_{xy} \ \hat{D}_{xz} \ D_{yy} \ \hat{D}_{yz} \ \hat{D}_{zz}]^T = [\mathbf{G}^T \mathbf{G}]^{-1} \mathbf{G}^T [\text{ADC}]$$

- Weighted LS (Multivariate Gaussian Noise):

$$[\hat{D}_{xx} \ \hat{D}_{xy} \ \hat{D}_{xz} \ D_{yy} \ \hat{D}_{yz} \ \hat{D}_{zz}]^T = [\mathbf{G}^T \Sigma^{-1} \mathbf{G}]^{-1} \mathbf{G}^T \Sigma^{-1} [\text{ADC}]$$

Challenges

$$-\frac{1}{b} \ln \frac{S_{dw}}{S_{ref}} = \mathbf{G}_g [D_{xx} \ D_{xy} \ D_{xz} \ D_{yy} \ D_{yz} \ D_{zz}]^T$$

- **Noise is not Gaussian**
 - Rician distributed observations
 - Bias at low SNR
 - Logarithm of the ratio with common reference
- Spatially varying noise
- Artifacts

A Likelihood Approach

Landman et al. 2007a

$$\frac{S_{dw}}{S_{ref}} = e^{-b\mathbf{g}^T \mathbf{D} \mathbf{g}}$$

Stejskal-Tanner Model

$$S_{ref} \sim \mathcal{R}(S_{ref0}, \sigma_{xy})$$

$$S_{dw} \sim \mathcal{R}(S_{ref0} e^{-b\mathbf{g}^T \mathbf{D} \mathbf{g}}, \sigma_{xy})$$

Rician
Likelihood
Model

$$\mathcal{L}(S_{dw_1} \dots S_{dw_n}, S_{ref}) = \mathcal{R}(S_{ref}, S_{ref0}, \sigma_{xy})$$

$$\prod_{i=1}^N \mathcal{R}(S_{dw_i}, S_{ref0} e^{-b\mathbf{g}_i^T \mathbf{D} \mathbf{g}_i}, \sigma_{xy})$$

$$\hat{\mathbf{D}} = \underset{\mathbf{D}, S_{ref0}, \sigma_{xy}}{\operatorname{argmax}} \mathcal{L}(S_{dw_1} \dots S_{dw_n}, S_{ref})$$

8 Unknowns

Reference Signal (x 1)

Noise Level (x 1)

Tensor Coefficients (x 6)



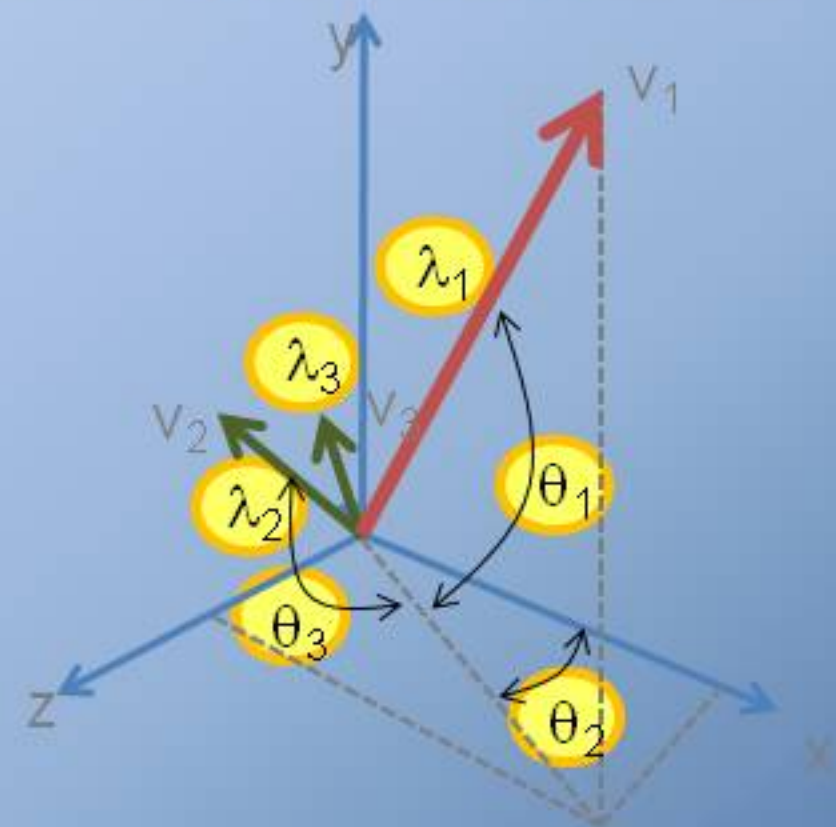
Tensor Parameterization

Landman et al. 2007a

Traditional Approach

$$\begin{aligned}
 D &= \begin{bmatrix} D_{xx} & D_{xy} & D_{xz} \\ D_{xy} & D_{yy} & D_{yz} \\ D_{xz} & D_{yz} & D_{zz} \end{bmatrix} \\
 &= R^T \begin{bmatrix} \lambda_1 & & \\ & \lambda_2 & \\ & & \lambda_3 \end{bmatrix} R \\
 &= [v_1 \ v_2 \ v_3] \begin{bmatrix} \lambda_1 & & \\ & \lambda_2 & \\ & & \lambda_3 \end{bmatrix} [v_1 \ v_2 \ v_3]^T
 \end{aligned}$$

Euler Angles and Eigenvalues



Proposed Approach

$$= R_{abc} \begin{bmatrix} e^{l_1} \\ e^{l_2} \\ e^{l_3} \end{bmatrix} R_{abc}^T$$

- Rodriguez parameters (a, b, c) based on quaternions
- Eigenvalue Logarithms

Mitigating Artifacts

Landman et al. 2008c

- **Incorrect noise levels**
 - Regularized noise field
 - Bayesian prior probabilities
 - Gaussian prior with mean set to the initial estimate and variance proportional to SNR^2
- **Influence of artifacts**
 - Truncated (Huberized) likelihood function
 - Determine truncation point adaptively from the initial likelihood distribution

$$\hat{D} = \underset{D, S_{\text{ref}0}, \sigma_{xy}}{\operatorname{argmax}} \mathcal{L}(S_{\text{dw}1} \dots S_{\text{dw}n}, S_{\text{ref}})$$



$$\hat{D} = \underset{D, S_{\text{ref}}, \sigma_{xy}}{\operatorname{argmax}} \mathcal{L}(S_{\text{dw}1} \dots S_{\text{dw}n}, S_{\text{ref}}) P(\sigma_{xy})$$



$$\hat{D} = \underset{D, S_{\text{ref}}, \sigma_{xy}}{\operatorname{argmax}} \mathcal{L}^*(S_{\text{dw}1} \dots S_{\text{dw}n}, S_{\text{ref}}) P(\sigma_{xy})$$

Diffusion Tensor Estimation by Maximizing Rician Likelihood (DTEMRL)

Landman et al. 2007a,2008c

$$\hat{D} = \underset{D, S_{\text{ref}}, \sigma_{xy}}{\operatorname{argmax}} \mathcal{L}^*(S_{d_{w_1}} \dots S_{d_{w_n}}, S_{\text{ref}}) P(\sigma_{xy})$$

Initialization

- Tensor
- Noise Level
- Reference Signal
- Noise Priors

Optimization

Tensor

$$\hat{D} = \underset{D}{\operatorname{argmax}} \mathcal{L}^*(\bullet; S_{\text{ref}}; \sigma_{xy}) P(\sigma_{xy})$$

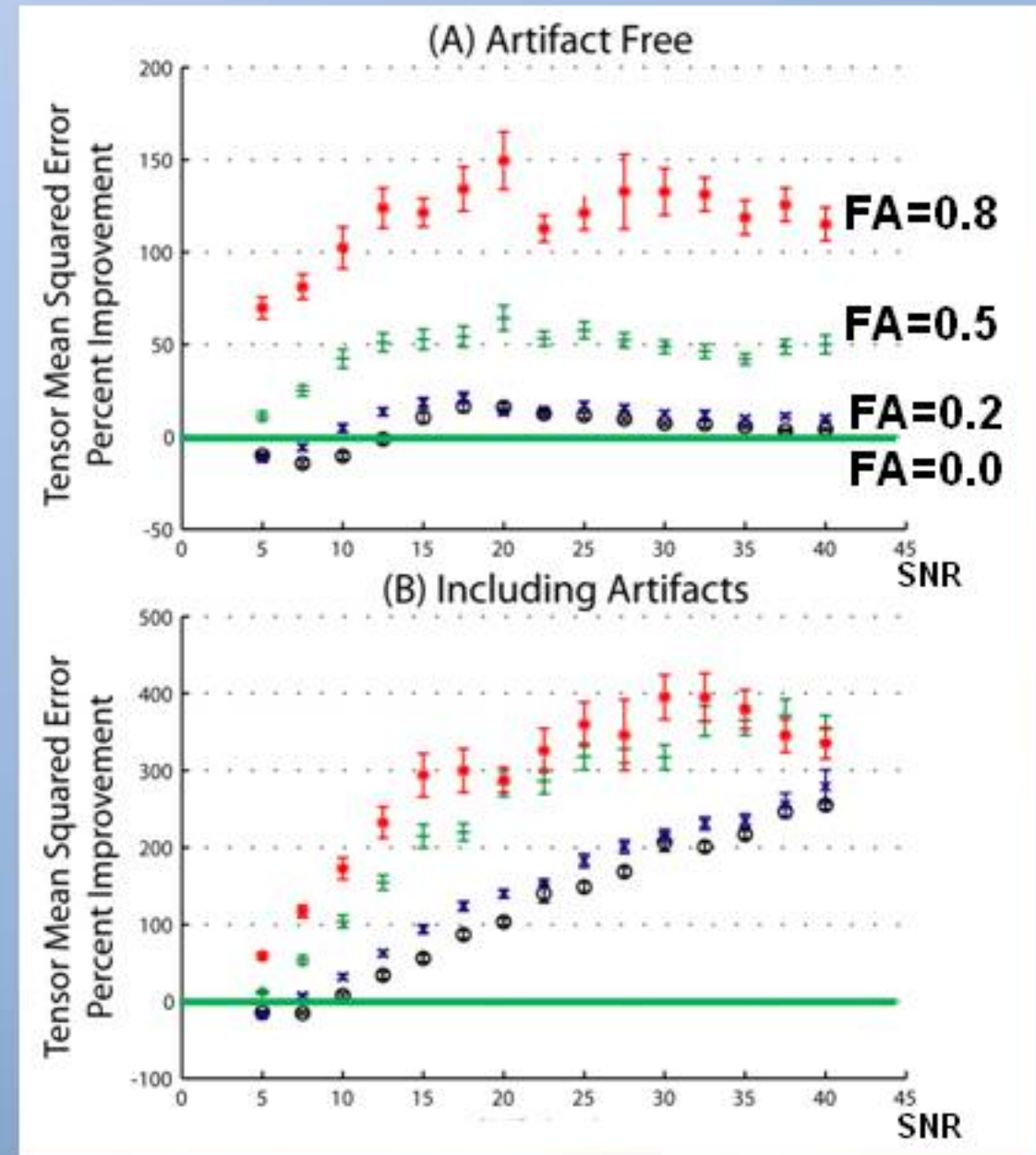
Imaging

$$\{\hat{S}_{\text{ref}}; \hat{\sigma}_{xy}\} = \underset{S_{\text{ref}}; \sigma_{xy}}{\operatorname{argmax}} \mathcal{L}^*(\bullet; \hat{D}) P(\sigma_{xy})$$

Reliability in Simulation

Landman et al. 2008c

- **Idealized (no Artifacts)**
 - Improvements in white matter above 10:1 SNR
 - Little effect on gray matter
- **Realistic (with Artifacts)**
 - Substantial improvements in both white matter and gray matter



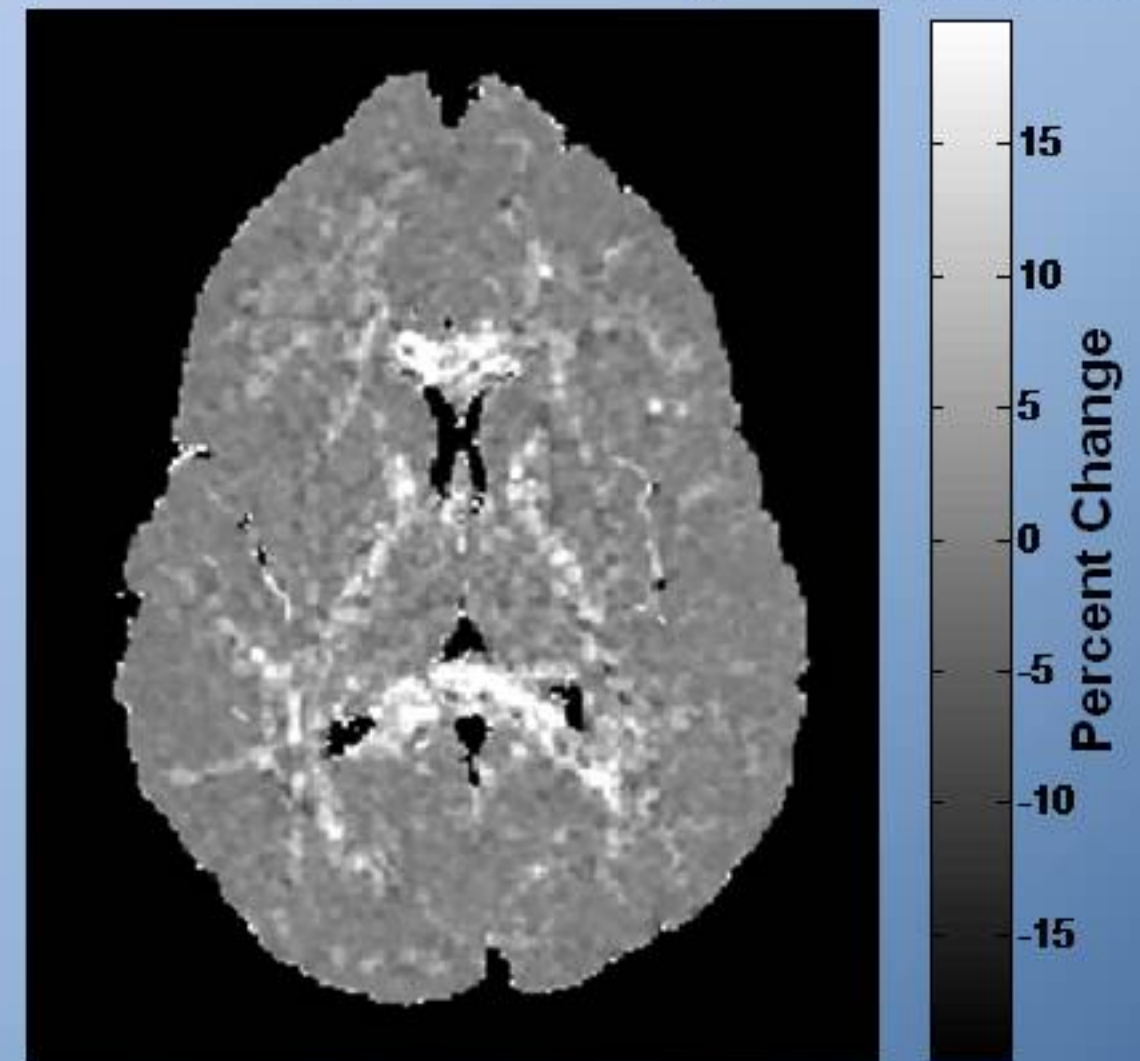
Reliability *In Vivo*

Landman et al. 2007a,2008c

- **Repeated Scanning**
 - One subject scanned 22 times over 3 days
- **Improved reproducibility in white matter**
 - 30%+ tensor coefficients
 - 15%+ FA
- **Little effect in gray matter**

FA Reproducibility

Improvement

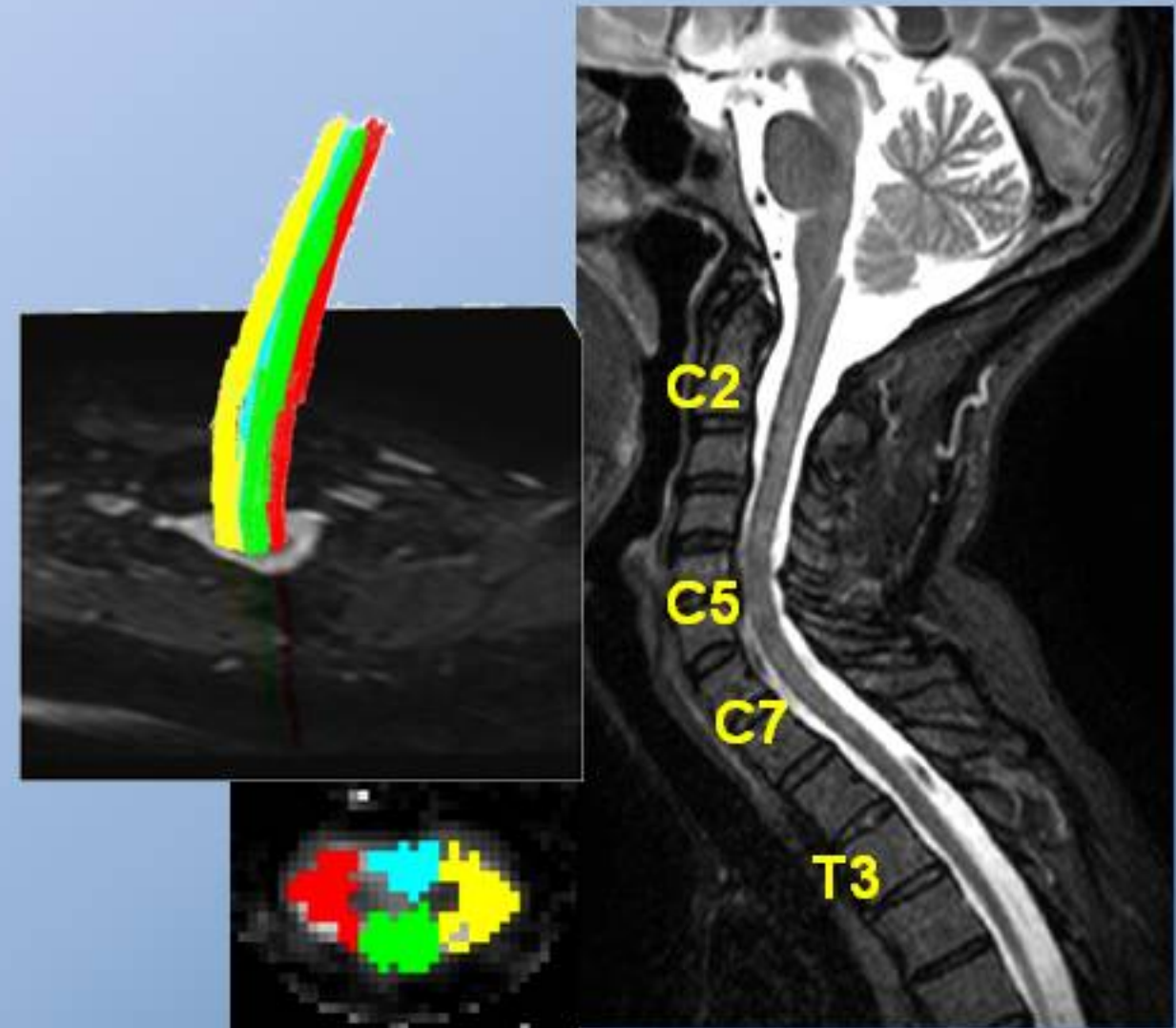


1.5T, b-value of 1000 s/mm², 30 DW directions

Spinal Cord DW-MRI

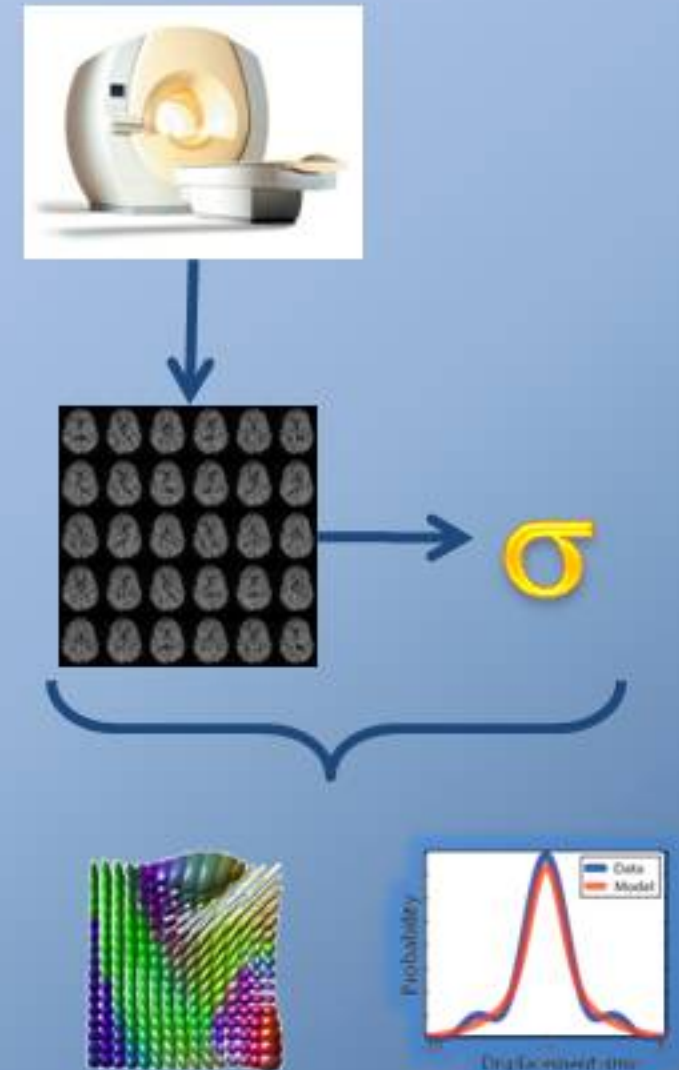
Smith et al. 2008

- **White matter in the spinal cord is highly oriented**
 - Orientation is known
 - Approximately radially symmetric
- **Can we learn more about the cellular environment?**



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- **Q-Space Imaging**
- Conclusion
- Future Directions



q-Space Imaging

Signal Attenuation

$$S(\mathbf{q}, \Delta) = S_0 \left| \iint \rho(\mathbf{r}_0) \mathbf{P}(\mathbf{r}_0 | \mathbf{r}, \Delta) \times \exp [j2\pi \mathbf{q} \cdot (\mathbf{r} - \mathbf{r}_0)] \right|$$

1D Nonparametric Stationary Propagator

$$S(q, \Delta) = S_0 \left| \int \mathbf{P}(\mathbf{r} - \mathbf{r}_0, \Delta) e^{j2\pi \mathbf{q} \cdot \mathbf{r}} d\mathbf{r} \right|$$

Observed Signal Reference Signal

Propagator Phase

q-Space Imaging

Signal Attenuation

$$S(\mathbf{q}, \Delta) = S_0 \left| \iint \rho(\mathbf{r}_0) \mathbf{P}(\mathbf{r}_0 | \mathbf{r}, \Delta) \times \exp[j2\pi \mathbf{q} \cdot (\mathbf{r} - \mathbf{r}_0)] \right|$$



1D Nonparametric
Stationary Propagator

$$S(q, \Delta) = S_0 \left| \int \mathbf{P}(\mathbf{r} - \mathbf{r}_0, \Delta) e^{j2\pi q r} dr \right|$$

Fourier transform

Amplitude Spectrum

- **Estimating the propagator**
 - Iterative reconstruction from amplitude spectrum
 - Assume phase \rightarrow inverse Fourier transform

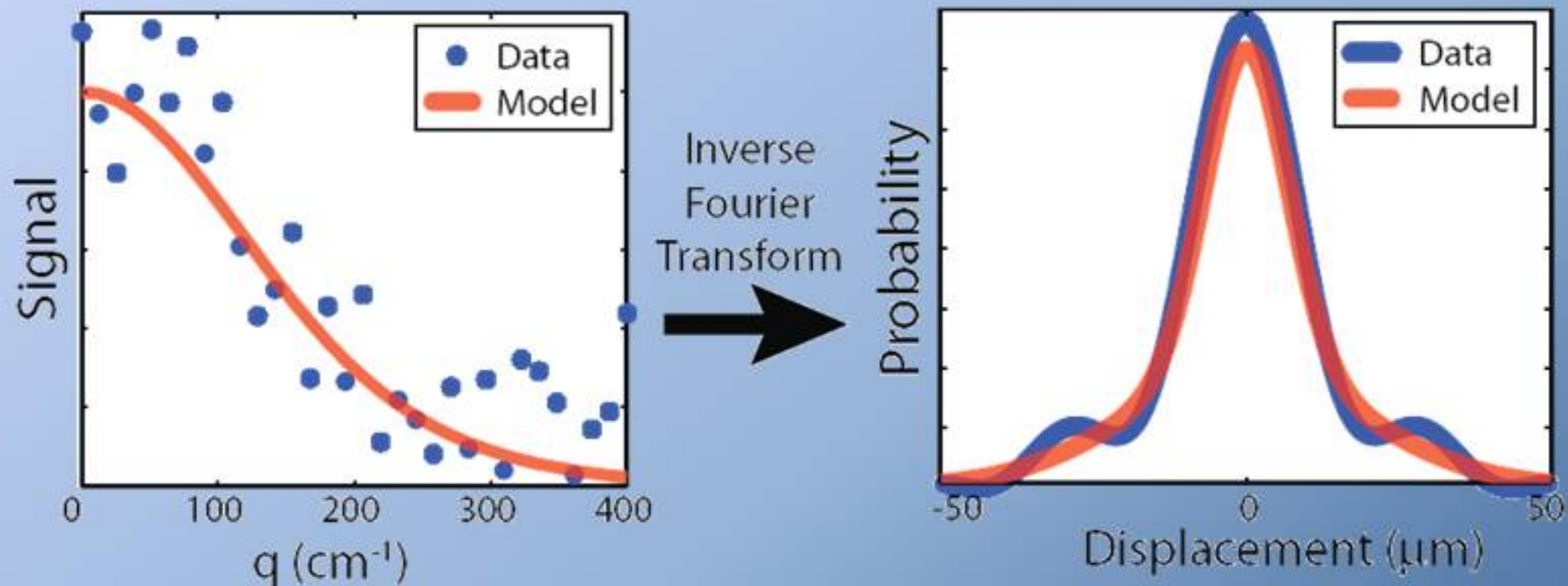
Assumptions

Norris 2001

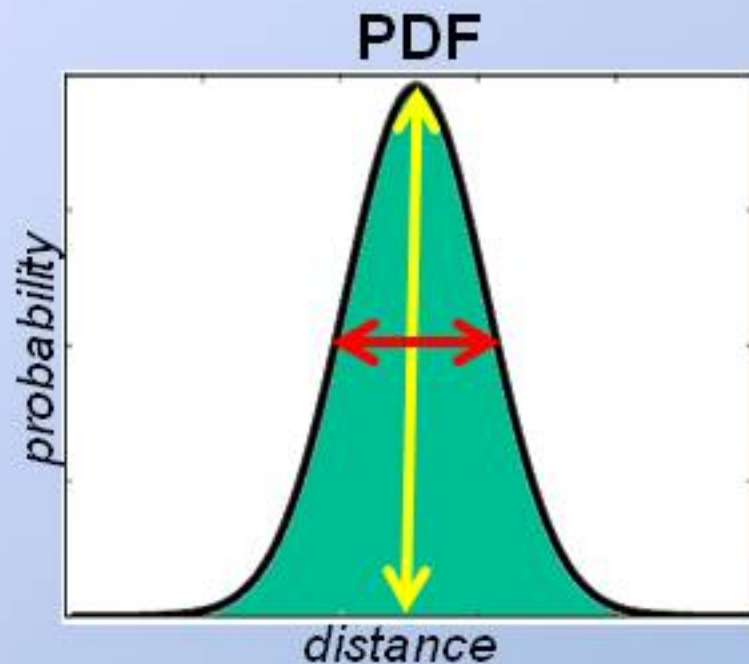
- “Long-time Limit”
 - With impermeable membranes and infinite diffusion time, the propagator becomes the autocorrelation of the restriction geometry
 - Zero Phase
- In practice for the CNS
 - Exchange is slow relative (100-600 ms) to diffusion time
 - Diffusion characteristic distances ($\sim 10 \mu\text{m}$) are greater than the spacing of cellular membranes (1-5 μm)
 - $\mathbf{P}(\mathbf{r} - \mathbf{r}_0, \tau) = S_0^{-1} \int S(q, \tau) e^{-j2\pi q r} d r$

q-Space Experiment

- Acquire $S(q, \Delta)$ at many values of q
- Smooth noisy data
- Take inverse Fourier transform



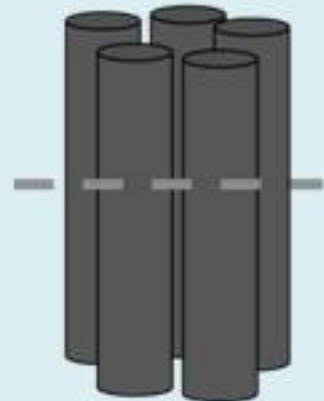
Clinical Contrasts



Contrasts

- Mode Probability (**P0**)
- Full Width at Half Maximum (**FWHM**)
- Root Mean Squared Displacement (**RMSD**)

Myelin Stain, Human C5



Healthy



“Loss of Myelin”



“Loss of Myelin and Axons”

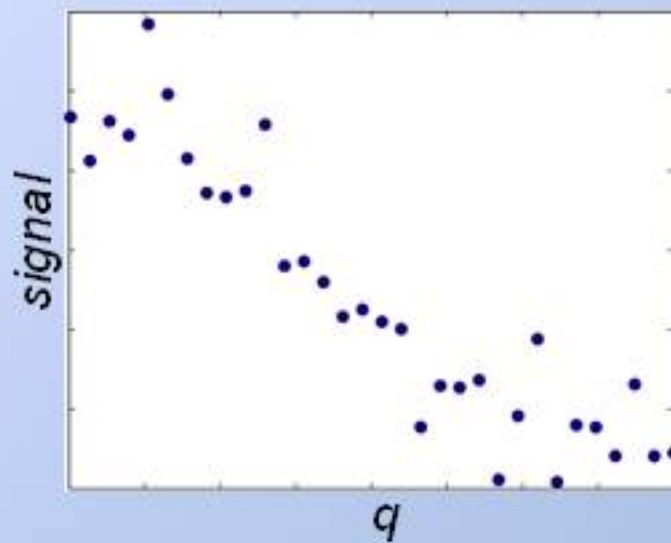


Pyramis 2004

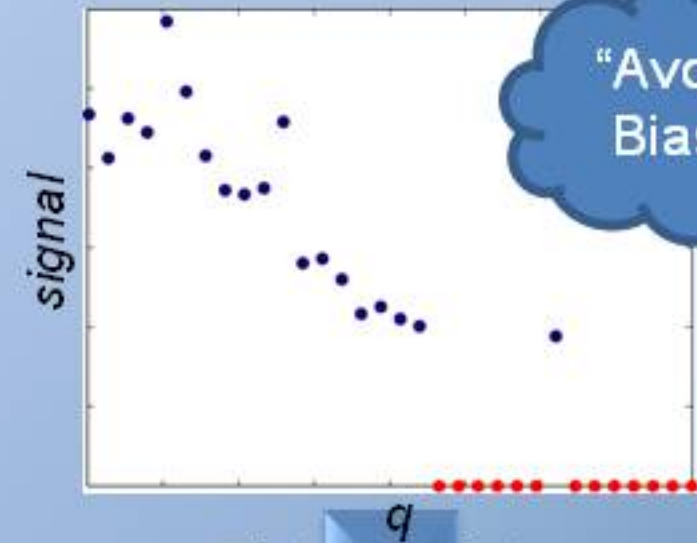
Traditional q-Space Approach

Cohen & Assaf 2002

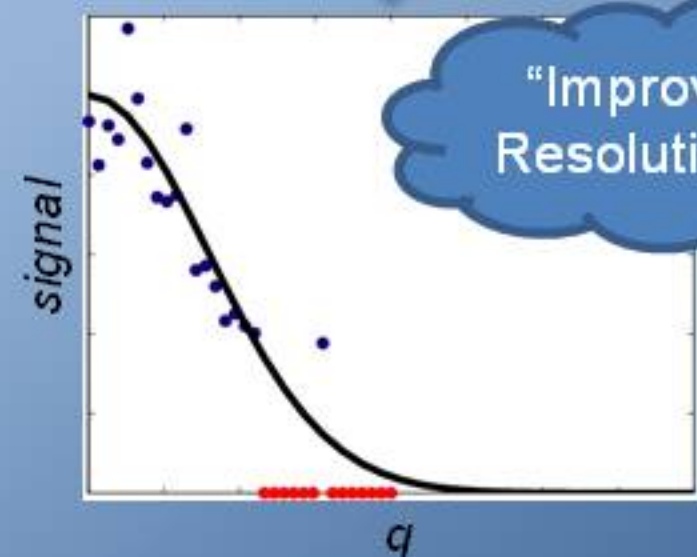
Observed Signal



Discard "Noise Floor"

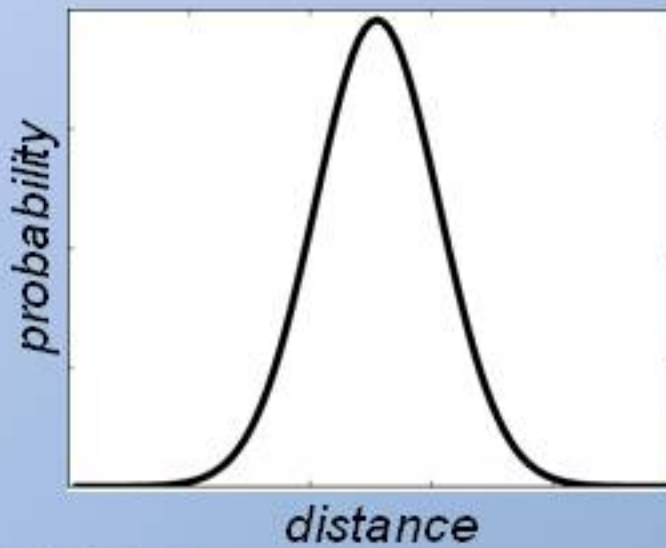


Extrapolate bi-Gaussian



Inverse Fourier transform

PDF



Challenges

$$S(q, \Delta) = S_0 \left| \int P(r, \Delta) e^{j2\pi qr} dr \right|$$

- **Ad hoc assumptions**
 - “Noise Floor” Criteria
 - Strict Model Fitting
 - Rician distributed observations
 - Bias at low SNR
- Limited acquisition
 - Cannot image *in vivo* at high q
 - Magnitude of spectrum of $P(r, \Delta)$
- Artifacts

A Likelihood Approach

Landman et al. 2008d

- **Properties of diffusion PDF's**
 - Positive } PDF
 - Symmetric } Physical constraints
 - Monotonic }
- **Model**
 - Positive mixture of zero-mean Gaussians
 - Estimate variances
 - Adaptively adjust model complexity
 - Determine number of basis functions with the L-curve criterion

Q-space Estimation by Maximizing Rician Likelihood: QEMRL

Landman et al. 2007a

$$S_{dw}(q) = S_0 \sum_i f_i e^{-kq^2 D_i}$$

$$\sum_i f_i = 1, \forall f_i \geq 0$$

$$D \in [3 \times 10^{-5}, 3 \times 10^{-3}] \text{ mm}^2/\text{s}$$

Mixture Model for Smooth PDF's

Constrain to Physiological Diffusivities

$$S_{dw} \sim \mathcal{R}(S_{\text{ref}0} e^{-kq^2 D}, \sigma_{xy})$$

$$\mathcal{L}(S_{dw_1} \dots S_{dw_n}, S_0) = \prod_{j=1}^N \mathcal{R}(S_{dw_j}, S_0 \sum_i f_i e^{-kq^2 D_i}, \sigma_{xy})$$

Rician Likelihood

$$\widehat{\{D\}} = \underset{\{D\}, S_0, \sigma_{xy}}{\operatorname{argmax}} \mathcal{L}^*(S_{dw_1} \dots S_{dw_n}, S_0) P(\sigma_{xy})$$

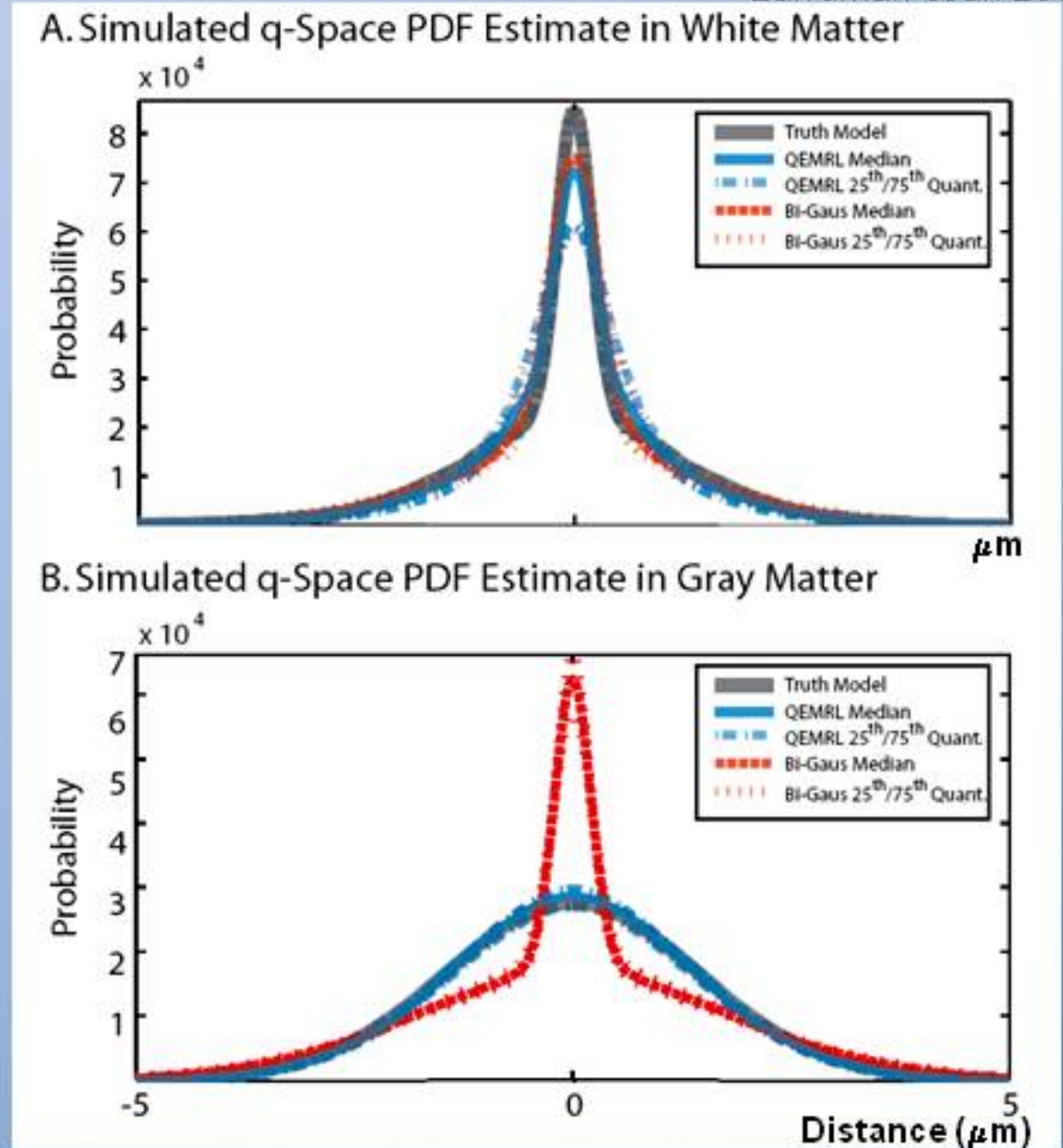
Truncated Likelihood and Bayesian Regularization

L-Curve Criteria to Select Number of Components

Reliability in Simulation

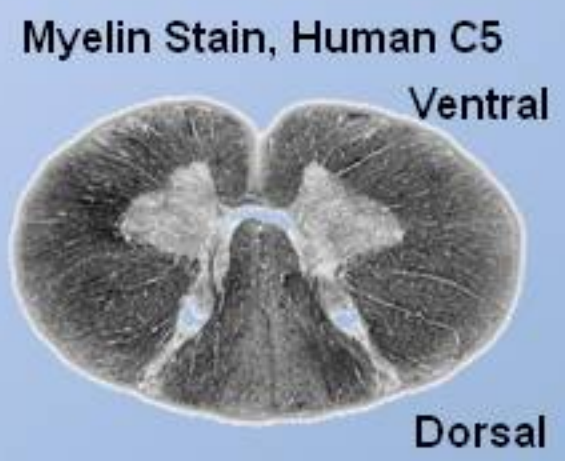
Landman et al. 2008d

- **Overall: 95%** improvement in integrated MSE of estimated PDF's
- **White matter: 21%** improvement
- **Gray Matter: 98%** improvement

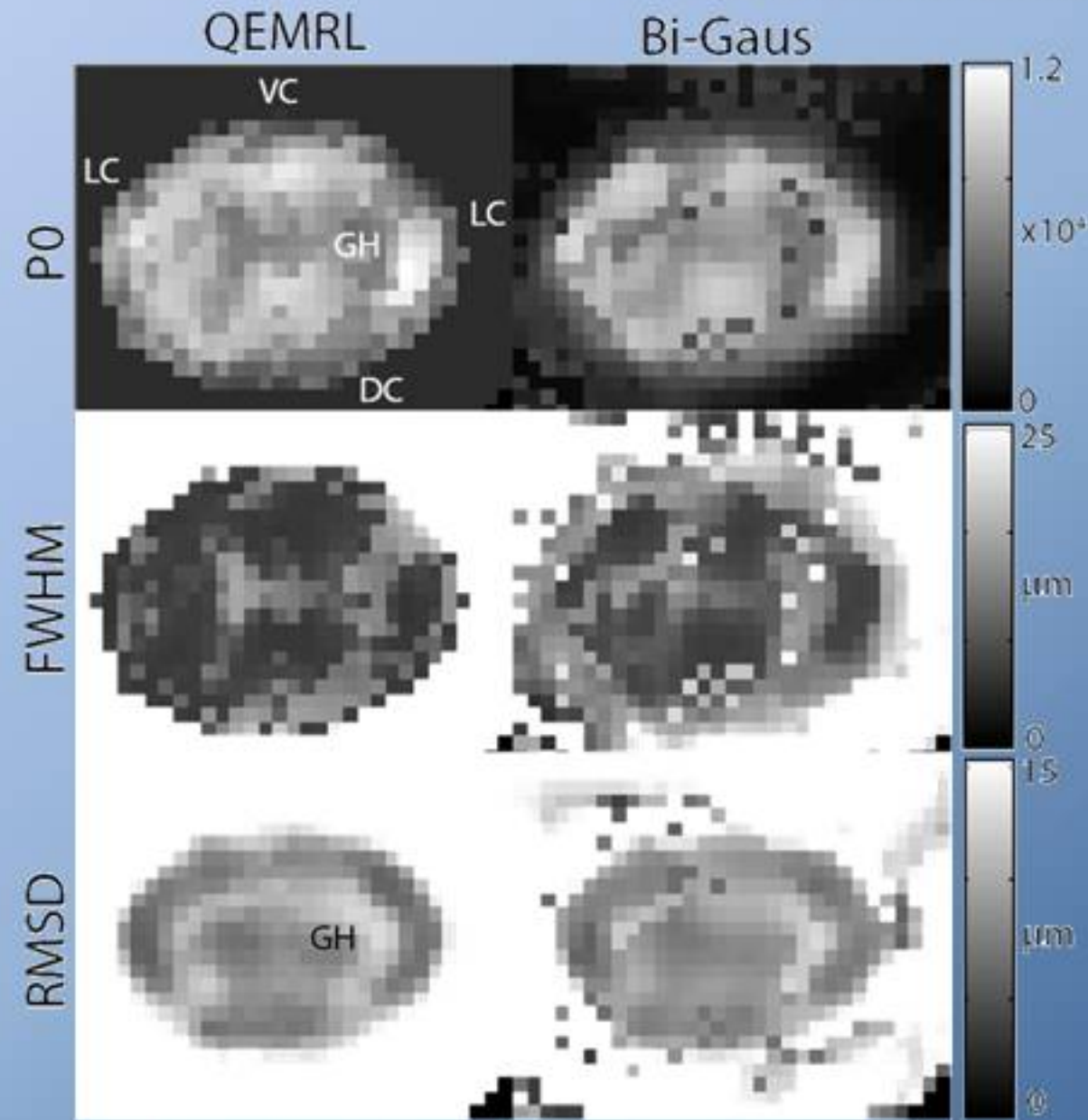
32 samples linearly spanning $q=0$ to 400 cm^{-1} at an SNR of 7:1

Reliability *In Vivo*

- **Improved reproducibility**
 - Mode Probability (**P0**) : **23%**
 - Full Width Half Maximum (**FWHM**) : **18%**
 - Root Mean Square Displacement (**RMSD**) : **26%**
- **Increased tissue contrast**



Landman et al. 2008d

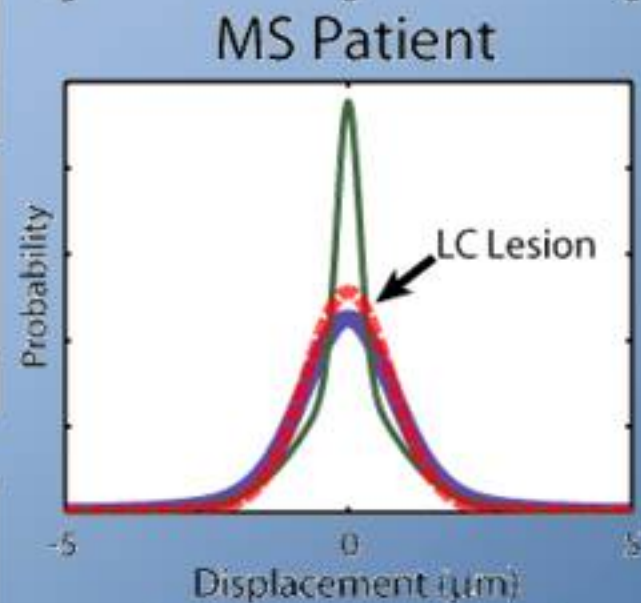
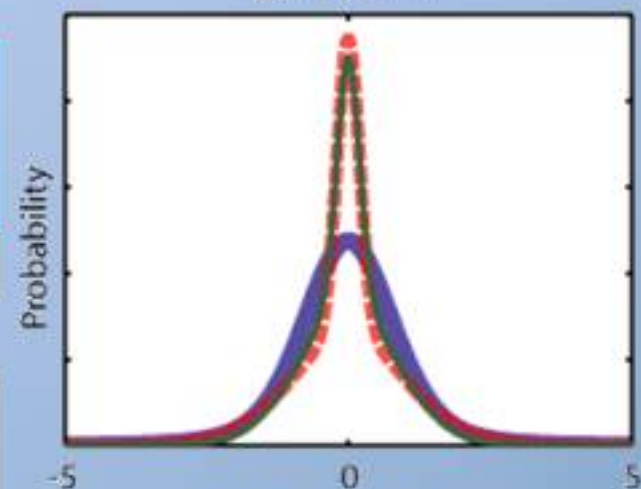
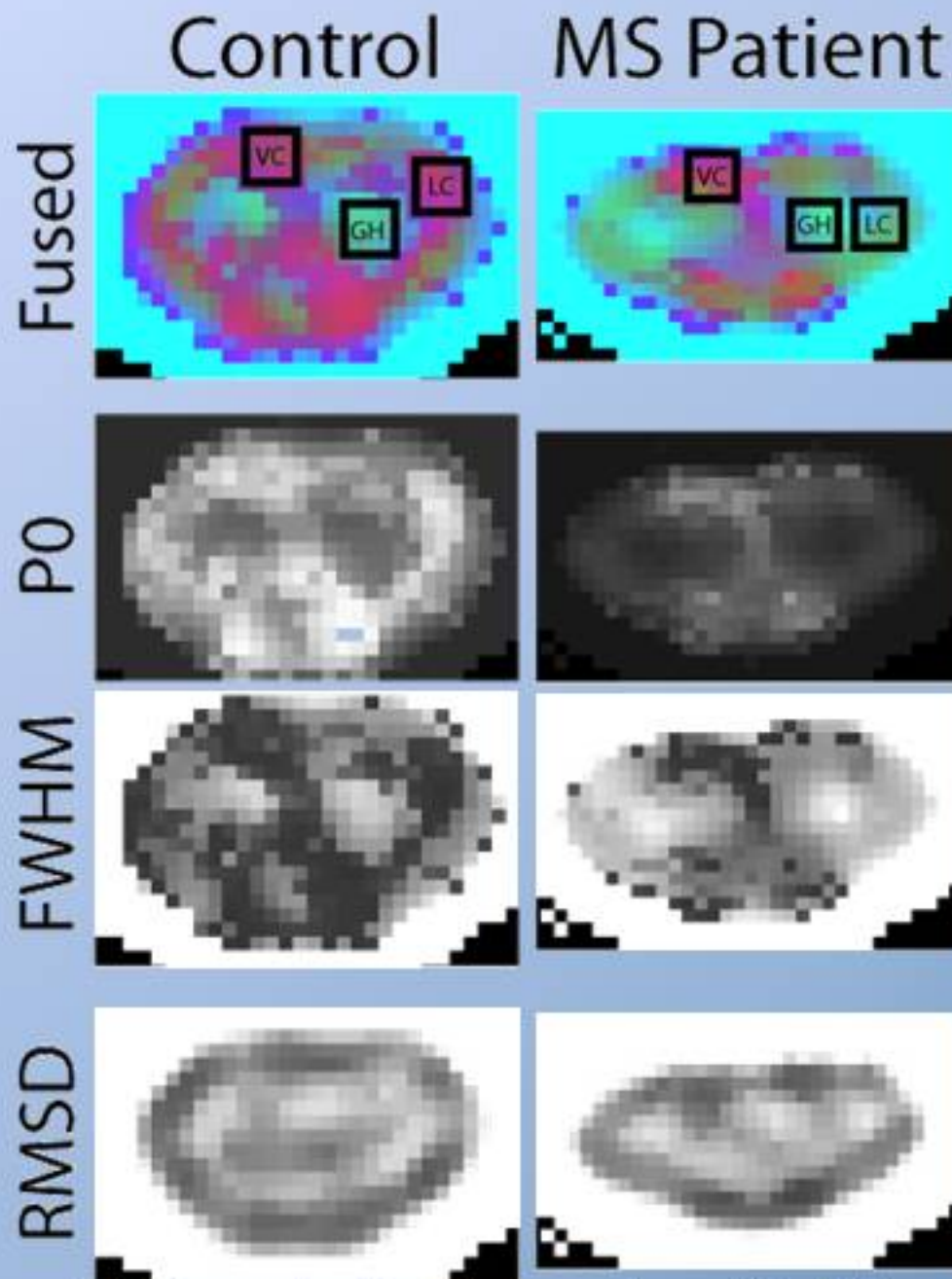


3T, 32 samples linearly spanning $q=0$ to 414 cm^{-1}
 SNR of $\sim 7:1$, $1.3 \times 1.3 \times 3.0 \text{ m}$

Potential Biomarkers for Multiple Sclerosis (MS)

Landman et al. 2008e

Myelin Stain, Human C5

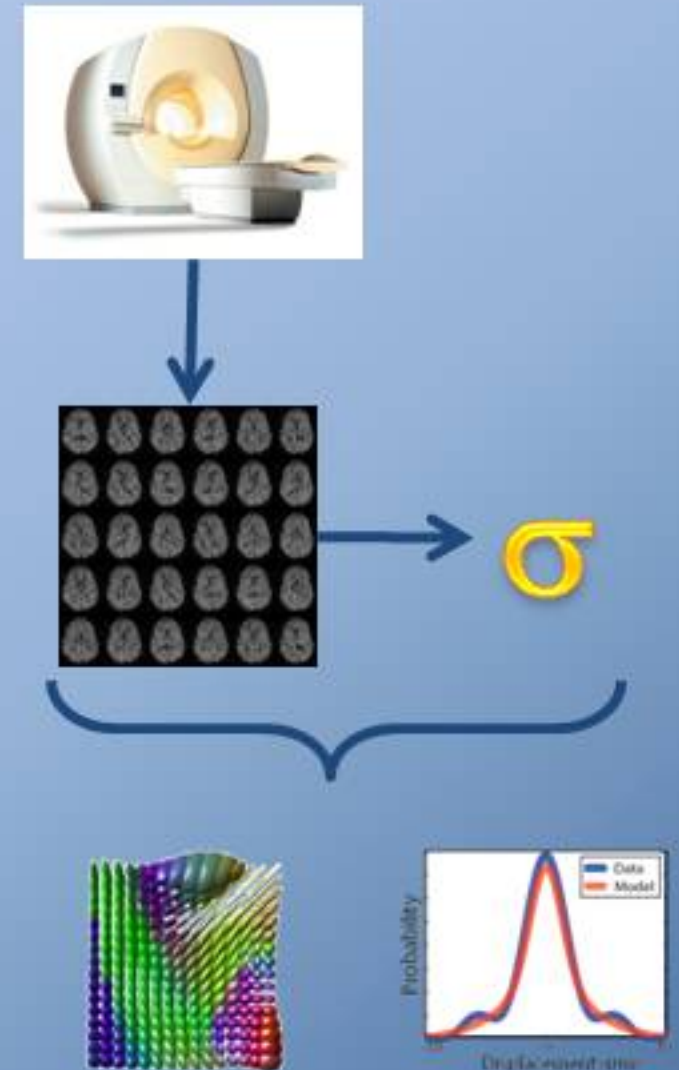


█ Gray Matter Horn (GH)
█ Ventral Column (VC)
█ Lateral Column (LC)

3T, 32 samples linearly spanning $q=0$ to 414 cm^{-1} , SNR of $\sim 7:1$, $1.3 \times 1.3 \times 3.0 \text{ m}$
 U.C. Berkeley EECS

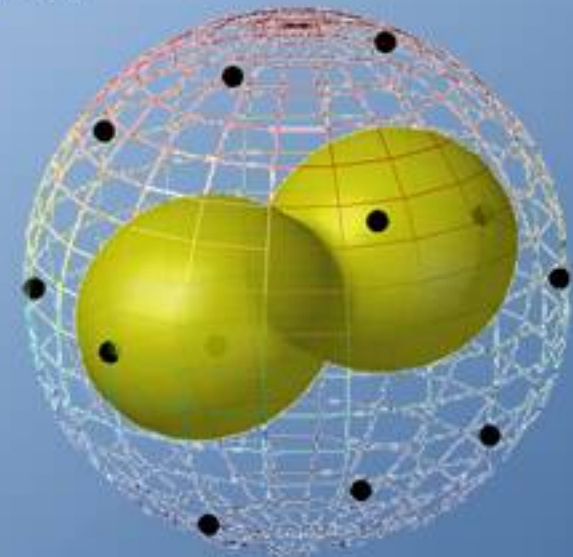
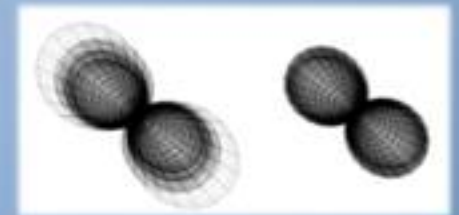
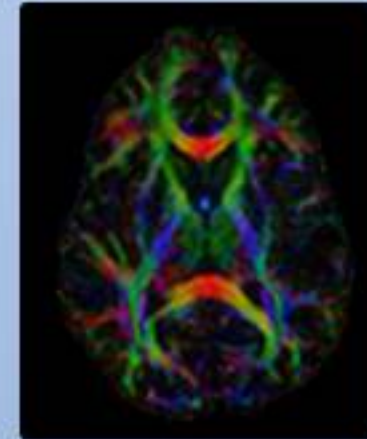
Overview

- Background
- Signal and Noise in DW-MRI
- Diffusion Tensor Imaging
- Q-Space Imaging
- **Conclusion**
- Future Directions



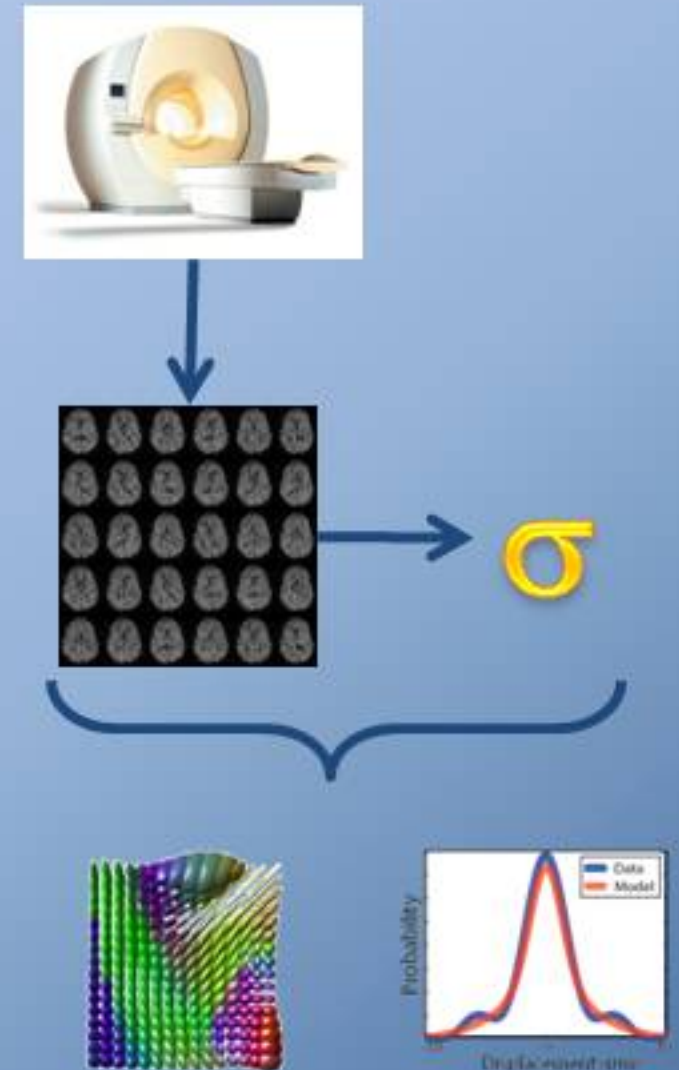
Conclusion

- **DW-MRI reveals cellular structure**
 - Rician noise corrupts analyses
- **Robust likelihood techniques**
 - Properly account for noise
 - Increase tissue contrast
 - Improve reliability
- **Likelihood models have great potential**
 - Forward applications: analysis
 - Reverse problems: acquisition design



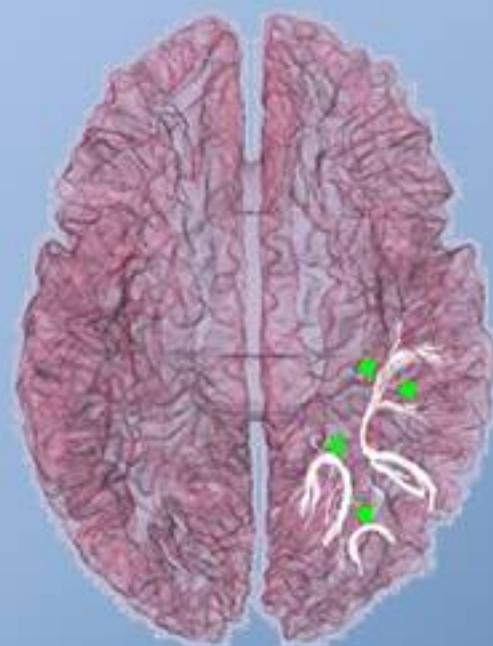
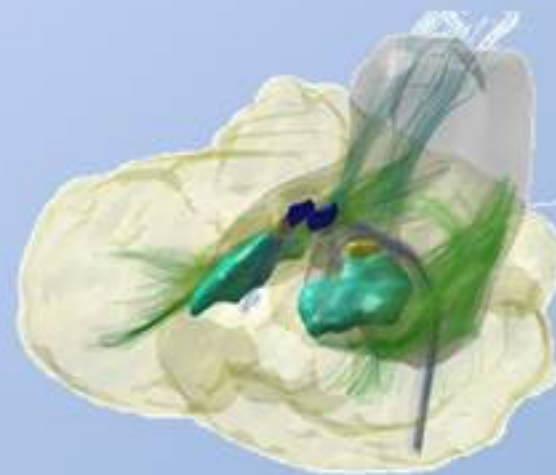
Overview

- Background
- Signal and Noise in DW-MRI
- Diffusion Tensor Imaging
- Q-Space Imaging
- Conclusion
- **Future Directions**



Clinical Applications

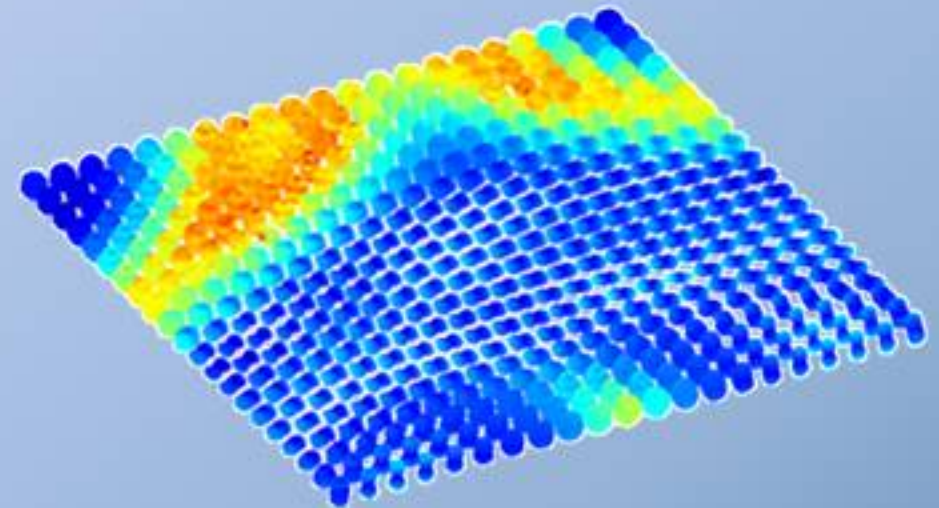
- Development of Biomarkers
 - MS lesion and normal appearing white matter
 - Spinocerebellar ataxia
- Targeted Acquisitions and Modeling
 - Spinal cord
 - MS/traumatic injury
 - Cerebellum/brainstem
 - Neurodegeneration
- Informatics



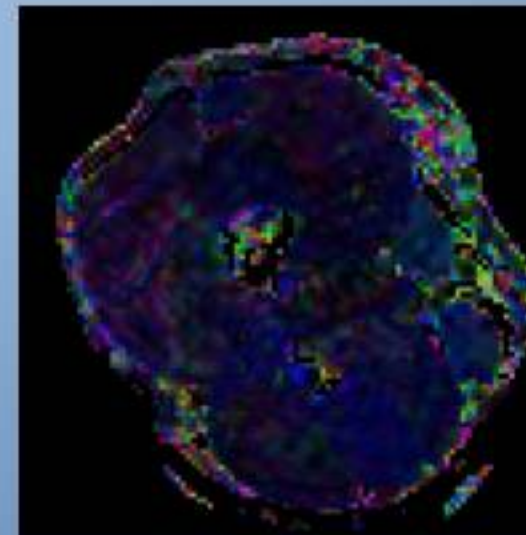
Emerging DW-MRI

- **Non-tensor DW-MRI**
 - High angular resolution
 - High q-value
 - Multiple b-values and directions
- **Non-traditional DW imaging targets**
 - Peripheral nerves
 - Musculoskeletal
 - Cardiac muscle

High Angular Resolution Diffusion Imaging

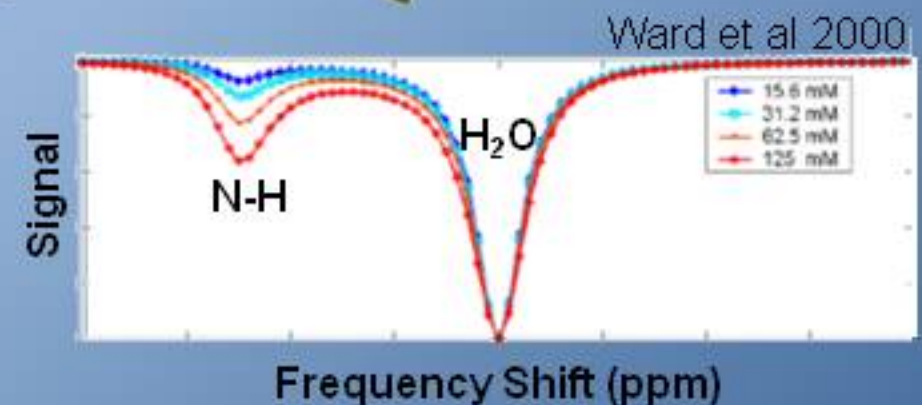
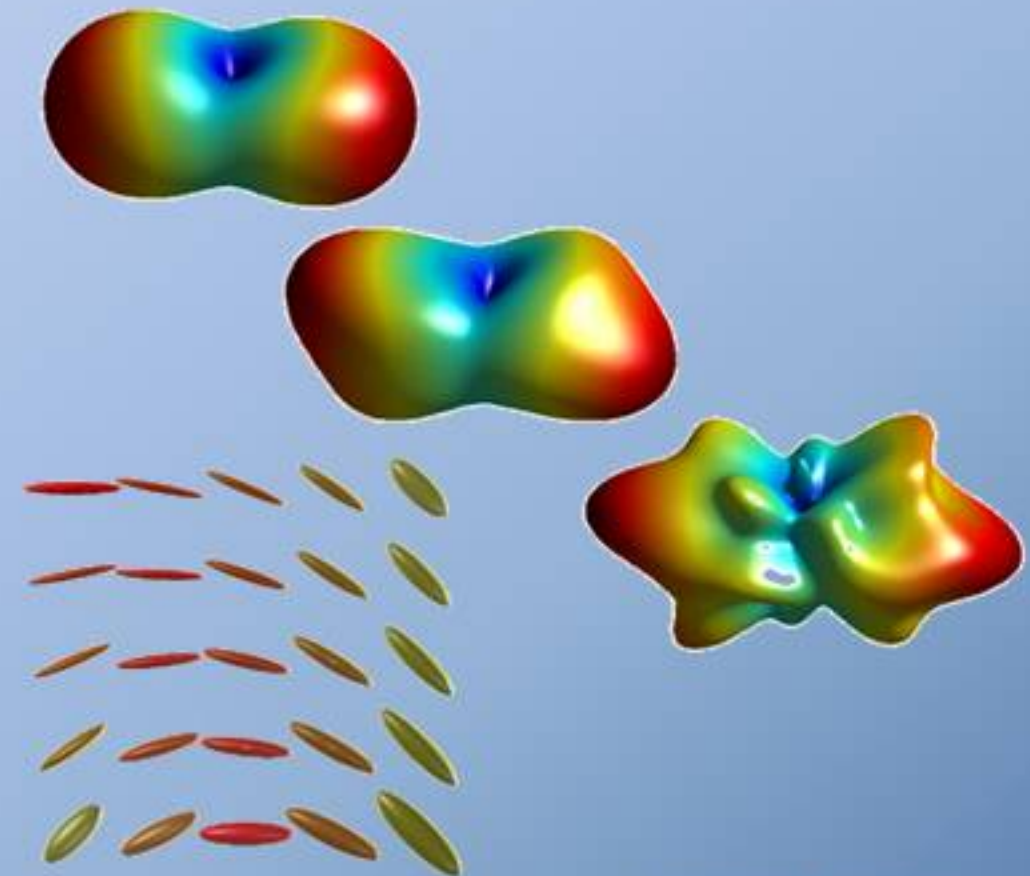


Musculoskeletal DW MRI



Statistical Analysis

- Hypothesis testing and model selection
 - Multi-dimensional/multi-modal characterization
 - Atlasing building
 - Interpolation
 - Metrics
- Quantitative Imaging
 - Metabolic imaging with Chemical Exchange Saturation Transfer (CEST)



Thank you.

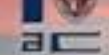
Thesis Committee

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Jerry Prince
Larry Schramm
Susumu Mori
Sarah Ying

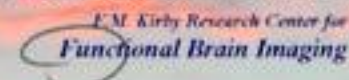
Research Groups



Image Analysis and Communications Lab



F.M. Kirby Research Center



Ataxia Research Center



Center for Magnetic Resonance Microimaging

In particular...

Alex Sinofsky
Amy Ruppel
Andrew Liu
Baohan Pan
Ewa Kulikowicz
Hao Huang
Harsh Agarwal
Howard Ying

Jay Burns
Jiangyang Zhang
John Bogovic
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Pelin Aksit
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Sue Eller
Shwetadwip Chowdhury
Stewart Mostofsky
Wade Mayes

Slides available at: <http://iacl.ece.jhu.edu/~bennett>

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- **Landman et al 2008a** : B. A. Landman, P-L. Bazin, and J. L. Prince, "Robust Diffusion Tensor Estimation by Maximizing Rician Likelihood," *International Society for Magnetic Resonance in Medicine*, Toronto, Canada, May 2008
- **Landman et al 2008b** : B. A. Landman, P-L. Bazin, J. L. Prince, "Robust Estimation of Spatially Variable Noise Fields: Applications to Diffusion Tensor Imaging", *NeuroImage*, Submitted February 2008
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- **Landman et al 2008d** : B. A. Landman, J. A.D. Farrell, S. A. Smith, P. C.M. van Zijl, and J. L. Prince, "Q-Space Diffusion Weighted MRI Analyzed with Maximizing Rician Likelihood Improves Reliability and Tissue Contrast," *International Society for Magnetic Resonance in Medicine*, Toronto, Canada, May 2008

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